



Gender associated muscle-tendon adaptations to resistance training

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Title: Gender associated muscle-tendon adaptations to resistance training

Short Title: Sex-specific muscle-tendon adaptations

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25 **Abstract**

26 **Purpose:** To compare the relative changes in muscle-tendon complex (MTC) properties
27 following high load resistance training (RT) in young males and females, and determine any
28 link with circulating TGF β -1 and IGF-I levels.

29 **Methods:** Twenty-eight participants were assigned to a training group and subdivided by sex
30 (T males [TM] aged 20 \pm 1 year, n =8, T females [TF] aged 19 \pm 3 year, n =8), whilst age-
31 matched 6 males and 6 females were assigned to control groups (ConM/F). The training
32 groups completed 8 weeks of resistance training (RT). MTC properties (Vastus Lateralis, VL)
33 physiological cross-sectional area (pCSA), quadriceps torque, patella tendon stiffness [K],
34 Young's modulus, volume, cross-sectional area, and length, circulating levels of TGF β -1
35 and IGF-I were assessed at baseline and post RT.

36 **Results:** Post RT, there was a significant increase in the mechanical and morphological
37 properties of the MTC in both training groups, compared to ConM/F (p <0.001). However,
38 there were no significant sex-specific changes in most MTC variables. There were however
39 significant sex differences in changes in K, with females exhibiting greater changes than
40 males at lower MVC (Maximal Voluntary Contraction) force levels (10% p =0.030 & 20%
41 MVC p =0.032) and the opposite effect seen at higher force levels (90% p =0.040 & 100%
42 MVC p =0.044). There were significant increases (p <0.05) in IGF-I in both TF and TM
43 following training, with no change in TGF β -1. There were no gender differences (p >0.05) in
44 IGF-I or TGF β -1. Interestingly, pooled population data showed that TGF β -1 correlated with
45 K at baseline, with no correlations identified between IGF-I and MTC properties.

46 **Conclusions:** Greater resting TGF β -1 levels are associated with superior tendon mechanical
47 properties. RT can impact opposite ends of the patella tendon force-elongation relationship in

48 each sex. Thus, different loading patterns may be needed to maximize resistance training
49 adaptations in each sex.

50 **Key words:** Dynamic, growth-factors, mechanical properties, muscle architecture

51

52 **Introduction:**

53 The muscle-tendon complex (MTC) exhibits multiple physiological characteristics which
54 differentially impact the physical capacities of males and females throughout the lifespan (1-
55 3) with young, exercising females possibly more susceptible to overuse injuries (such as
56 tendinopathies) than males (4).

57 In particular, there is increasing evidence of sex-specific chronic adaptations of the in-series
58 elastic component to resistance training (RT), over and above the intrinsic gender differences
59 in both the absolute MTC properties at rest, and its acute response to exercise. Indeed,
60 differences in viscoelastic properties of the free tendon and tendon-aponeurosis between
61 young males and females have been demonstrated (5-7), with females displaying lower
62 stiffness, modulus, hysteresis and greater strain. The combination of data from previous
63 studies (8, 9) highlight the difference in both resting and post-exercise tendon collagen
64 fractional synthetic rate (FSR) between males and females, with FSR remaining significantly
65 elevated 72 hours post 60 minutes leg-kicking, endurance type exercise in males. Further
66 research has also shown that gender additionally influences the post resistance-exercise
67 expression of tendon structural and extracellular matrix (ECM) regulatory components (10).

68 The sex difference in responsiveness to training in chronic response terms is highlighted in
69 Westh et al.(11) who showed that long-term habitually trained young female runners
70 displayed significantly lower tendon stiffness compared to similarly trained male runners.
71 Interestingly however, these chronically trained female runners did not differ significantly in
72 terms of tendon morphology or mechanical properties to female non-runners, which raises

73 any questions with regards to any change in the intrinsic quality of the tendon with chronic
74 training in females. It is also notable that sex differences have been demonstrated in the
75 adaptability of MTC properties following an extended period of physical training in older
76 individuals (12, 13), thereby emphasising the persistent nature of the superior responsiveness
77 and adaptability in males. Whilst research strongly suggests that females demonstrate
78 dissimilar relative adaption profiles to tendon mechanical stimuli compared to age-matched
79 male counterparts, the adaptability and endocrine links associated with this observation
80 following heavy load dynamic resistance training of tendon for instance, have yet to be
81 elucidated.

82 *In vitro* work suggests of particular importance to the endocrine adaptation of tendon, are
83 growth factors Transforming Growth Factor Beta – 1 (TGF β -1) and Insulin-Like Growth
84 Factor One (IGF-I). Their primary roles in tendon include proliferation and migration of
85 fibroblasts, subsequently increasing the production of collagens and other extracellular matrix
86 structures in these cells during the remodelling stages (14, 15). In humans (16) direct
87 administration of IGF-I enhanced the collagen fractional synthetic rate in young and older
88 males. In parallel, administration of IGF-I plus TGF β -1 together, significantly improved
89 mechanical properties of rabbit tendon (17). Recent work from Astill et al. (18) demonstrates
90 that following an acute bout of RT, males and females both display significantly elevated
91 IGF-I levels 3 hours post RT. However, only females had significantly elevated peritendinous
92 levels of IGF-I at 4 hours post, whereas males did not. Additionally, males showed greater
93 post-RT changes in Matrix Metalloproteinase 9 (MMP-9) levels than females, and females
94 had a more prolonged exercise-induced elevations in tissue inhibitor of metalloproteinases-I
95 (TIMP-I) than males.

96 Data shows no normative difference when comparing circulating TGF β -1 levels in males, pre
97 and post-menopausal females, and pregnant females (19, 20). Additionally, to the authors'

98 knowledge, there is no evidence to show that in a young, healthy population, there are
99 marked fluctuations in systemic TGF β -1 levels (21). At present, the literature on any link
100 between the previously reported (22) acute *in vivo* TGF β -1 response to mechanical loading,
101 and the magnitude or nature of human MTC training adaptations is limited. A topical study is
102 that of Heinemeier et al. (22) who found elevation in systemic TGF β -1 levels (30%)
103 following 1 hour of uphill (3%) treadmill running at 12kph in young persons, which the
104 authors proposed may have been linked to the observed change in peri-tendon TGF β -1 levels
105 and hence regulation of Type I collagen synthesis. However, in this Heinemeier et al.'s study,
106 the exercise protocol involved endurance running, and hence, arguably, a less than optimal
107 training modality (compared to heavy resistance exercise) where the outcome aimed for is
108 inducing MTC adaptations (23).

109

110 Taking the observed differences between sexes in MTC response/ adaptability to physical
111 stimuli, no study to date has characterised the sex-specific adaptations of the MTC, following
112 a period of heavy dynamic resistance training. In addition, it remains unclear whether any
113 difference would be associated with major growth-factor candidates purported to influence
114 MTC properties and adaptations to training. Therefore, the objectives of this study were to 1).
115 Characterise the MTC adaptation to a period of dynamic, heavy-load resistance training in
116 males and females, 2) identify any sex-related differences across MTC properties and 3)
117 investigate whether any of the adaptive responses could be reflected in changes in two key
118 circulating growth factors related to the MTC.

119

120

121 **Methods:**

122 *Participants:*

123
124 Twenty-eight young participants recruited from the local university campus, gave written
125 informed consent to participate in the study. All procedures and experimental protocols were
126 approved by the Manchester Metropolitan University Cheshire Campus ethics committee.
127 Exclusion criteria included the presence of any known musculoskeletal, neurological,
128 inflammatory, or metabolic disorders or injury. Participants took part in recreational activities
129 such as team sports and had either never taken part in lower limb resistance training or had
130 not done so within the previous 12 months. Each participant completed a physical activity
131 diary, outlining that they each habitually completed 3-5 hours of non-resistance based
132 moderate physical activity per week. Sixteen participants were then equally subdivided by
133 sex and randomly assigned to a training group (T males [TM] age 20 ± 1 years, mass 81 ± 4 Kg,
134 T females [TF] age 19 ± 3 years, mass 69 ± 3 Kg), whilst 6 males ([ConM] age 22 ± 2 years, mass
135 82 ± 2 Kg) and 6 females ([ConF] age 23 ± 4 , mass 63 ± 4 Kg) were assigned to a control group
136 (CON). All females were eumenorrheic (menstrual cycle duration of 26-30 days) and none
137 used any form of Oral Contraceptive Pill, the latter having been shown to impact of the MTC
138 properties in females (24).

139

140 *Study Design:*

141

142 The study design was convenience sampling, with participants separated into groups
143 according to sex followed by random allocation to one of two groups (i.e. training or control).
144 Following familiarisation with laboratory procedures at least one week prior to testing proper,
145 participants were assessed for MTC morphology/functional properties and growth factors at
146 baseline (week 0). Measurements were repeated after 8 weeks resistance training (post-
147 training).

148

149

150 *Muscle Physiological Cross-sectional Area (pCSA):*

151

152 The measurement techniques used for the calculation for physiological cross-sectional area of
153 the *Vastus Lateralis* (VL) muscle in the current study have been documented elsewhere (25,
154 26). Briefly, multiple anatomical cross-sectional area (aCSA) measures were made via
155 brightness mode ultrasonography (7.5-MHz, 40mm array probe, AU5, Esaote Biomedica,
156 Genoa, Italy) at 25%, 50% and 75% along the length of the VL muscle (insertion to origin),
157 together with pennation angles and fascicle lengths. Muscle volume was then calculated
158 using the truncated cone method, which has been validated in a number of previous studies
159 (27, 28). VL pCSA was calculated by dividing muscle volume by fascicle length (28).

160

161 *Quadriceps Torque:*

162

163 Maximal isometric knee extension torque was measured with the knee at 50° knee flexion
164 (full knee extension = 0°) on the right leg of all participants. This angle was chosen to fall at
165 50% of the range of motion covered during the exercise routines, thereby minimising the
166 effect of muscle length specificity on the reported muscle torque increments. After a series of
167 warm up trials consisting of ten isokinetic contractions at 60°·s⁻¹ at self-perceived 50-85%
168 maximal effort, participants were instructed to rapidly exert maximal isometric force
169 (maximal voluntary contraction, MVC) against the dynamometer (Cybex, Phoenix
170 Healthcare, UK) lever arm. Joint torque data traces were displayed on the screen of a
171 MacBook Air computer (Apple Computer, Cupertino, CA, USA), which was interfaced with
172 an A/D system (Acknowledge, Biopac Systems, Santa Barbara, CA, USA) with a sampling

173 frequency of 2000 Hz. Isometric contractions were held for ~2 s at the plateau with a 60 s
174 rest period between contractions. Peak torque was expressed as the average of data points
175 over a 500 ms period at the plateau phase (i.e. 250 ms either side of the instantaneous peak
176 torque). The peak torque of three extensions was used as the measure of torque in each
177 participant.

178

179 *Estimation of Co-Contraction from Electromyographical Activity:*

180

181 A pair of Ag-AgCl electrodes (Neuroline 720, Ambu, Denmark), were placed on clean,
182 shaved, and abraded skin, at 50% of femur length, in the mid-sagittal plane of the biceps
183 femoris. The reference electrode (Blue sensor L, Ambu, Denmark) was placed on the lateral
184 tibial condyle. The raw EMG signal was preamplified (MP100, Biopac Systems Inc., USA),
185 amplified $\times 1000$ (MP100, Biopac Systems Inc., USA), bandpass filtered between 10-500 Hz
186 (Biopac Systems, USA) with a notch at 50Hz, and sampled at 2000 Hz. All EMG and torque
187 signals were displayed in real time in AcqKnowledge software (Biopac systems Inc., USA)
188 via a PC. Two maximal knee flexion contractions were carried out to obtain the EMG at
189 maximal flexion torque. The root mean square (RMS) EMG activity was averaged for a
190 500ms period (average of 1.5ms moving windows) which coincided with the plateau of peak
191 torque.

192 To reiterate, the EMG of the long head of the biceps femoris muscle was measured to
193 ascertain the level of antagonist muscle co-contraction during the required isometric knee-
194 extension performances. The biceps femoris torque during a knee-flexion contraction was
195 calculated as described by McMahon et al. (25) whereby a linear relationship between BF

196 EMG and torque is assumed, thus enabling the quantification of the ‘pull back torque’ during
197 knee extensions, and ultimately, the total forces experienced by the patella tendon (29, 30).

198

199 *Tendon Properties:*

200 The measures of tendon properties used in the current investigation have been described
201 elsewhere (31). Briefly, tendon elongation was determined using brightness mode ultrasound
202 imaging over the apex of the patella in the sagittal plane, with the knee fixed at 90⁰ flexion as
203 per the norm in *in vivo* tendon properties assessment. Five preconditioning trials were carried
204 out to ensure reproducibility. Following this, three ramped, 6-second isometric contractions
205 were monitored for the distance between the original position of the tissue under the skin,
206 relative to the new position of the tissue using ultrasound images captured onto a personal
207 computer at 25 Hz. The ultrasound output was synchronized using a square wave signal
208 generator to allow temporal alignment with both torque and EMG data. Tendon displacement
209 was determined at intervals of 10% of the maximal force (from 10% to 100%) using image J.
210 Three efforts were analysed, and the average reported as the profile of tendon force versus
211 elongation for the participant. The plotted force–elongation relationship was fitted with a
212 second-order polynomial function, forced through zero. Instantaneous tendon stiffness (K)
213 values were calculated from the slope of the tangents at 10% force intervals (30). Mean
214 tendon stiffness was the average stiffness value from 10-100% MVC.

215

216 Patellar tendon (PT) resting length (TL) and cross-sectional area (Tcsa) were also assessed
217 with the knee joint at 90⁰ of flexion. TL was measured from the inferior pole of the patellar to
218 the superior aspect of the tibial tuberosity determined from sagittal-plane ultrasound images.
219 Tcsa was determined from the mean of transverse plane ultrasound images taken at 25%,

220 50%, and 75% TL. Young's modulus (E) was computed as instantaneous stiffness multiplied
221 by the ratio of resting TL/Tcsa. Mean tendon stiffness was the average stiffness value from
222 10-100% MVC.

223 PT volume (TVol) was calculated using the TL and Tcsa values along the length of the
224 tendon using the truncated cone method, which used the same principles as those
225 demonstrated on muscle volume assessments (27).

226

227 *Circulating Growth Factor Levels (IGF-I and TGF β -1)*

228

229 Pre and post-training, following an overnight fast, (~10 hours), participants reported to the
230 laboratory between 9-11am. 5 mL blood samples were collected from the antecubital vein of
231 the forearm, placed in a crushed ice bed for 1.5 to 2-hours, and then centrifuged at 4°C for 10
232 min at 4,800 rpm, with the supernatant being removed and stored in at least two aliquots in
233 eppendorfs at -20° Celsius for later analysis. IGF-I and TGF β -1 were analysed using the
234 standard enzyme-linked immuno-sorbent assay (ELISA) procedure, as described by
235 McMahan et al. (31), with the overnight incubation for the first antibody binding phase
236 option for the TGF β -1 (thereby increasing the sensitivity of the readings). Post-training
237 samples were taken 3-4 days post final training session, at the same time-of-day as the pre-
238 training sampling for each participant.

239

240 The laboratory tests were timed to avoid diurnal variability or acute exercise-induced growth
241 factor fluctuations.

242

243 *Resistance Training*

244

245 Resistance training (RT) was performed three times per week for 8 weeks at 80% of 1
246 repetition maximum (1RM) on the knee extensor complex. Exercises included the back squat,
247 leg press, leg extension (Technogym, Berkshire, UK), lunge, Bulgarian split squat and
248 Sampson chair. All exercise sessions were supervised by a member of the research team.
249 Participants completed two familiarisation sessions at 70% 1RM prior to commencing the
250 resistance training program. 1RMs were measured at baseline and every 2 weeks, with
251 loading weight progressed. Volume (i.e. repetitions and sets) was identical for each training
252 group, with each training session consisting of four exercises and performing three sets of 10
253 repetitions per exercise for the first 4 weeks, and four sets of eight repetitions per exercise
254 thereafter. Training sessions would typically last ~60 minutes, with training records being
255 diligently completed during sessions.

256

257 *Statistics:*

258

259 Statistical analysis was carried out using IBM SPSS v19 (IBM Inc, USA). Data was analysed
260 using a 4×2 ANCOVA with baseline measures used as covariates. The within-group factor
261 was the phase of training (baseline, post-training) and the between-group factor was training
262 group (i.e. TM, TF, ConM, ConF). Post-hoc comparisons are Bonferroni corrected and
263 adjustments for multiple comparisons are applied in the correlation tables. All data are
264 presented as mean ± standard error of the mean (SEM). Statistical significance was set with
265 alpha at ≤ 0.05 . Power (β) and effect size (ES) are reported for those changes that exhibited
266 significant sex differences, where power was calculated post hoc using the independent t-test
267 assumptions. The sample size required to identify sex differences in the morphological and
268 mechanical properties of the MTC was deemed adequate given that achieved study power
269 was ≥ 0.8 .

270

271

272 **Results:**273 *Sex differences at baseline*

274 There were no significant sex differences ($p>0.05$) in pCSA, Tvol , Tcsa, TL , PT K, PT E,
275 TGF β -1 or IGF-I. As expected however, TM produced significantly ($p<0.01$) greater torque
276 than TF.

277

278 *MTC Properties changes*

279 There were significant increases in pCSA, strength, PT Vol, mean PT K and E , and IGF-I
280 (see Table 1) in each training group, with no sex differences. However, when PT K was
281 analysed at discrete force regions, significant sex-specific differences were identified (see
282 Figure 1). TF had significantly greater increments in stiffness compared to TM following
283 training at lower MVC forces (10% ($p=0.030$, β 0.94, ES 0.29) and 20%MVC ($p=0.032$, β
284 0.93, ES 0.28)), whereas TM had significantly stiffer tendons compared to TF at higher MVC
285 forces (90% ($p=0.040$, β 0.92, ES 0.24) and 100% ($p=0.044$, β 0.79, ES 0.26)). There were no
286 changes in TGF β -1 in either the training groups (see Table 1), or either of the control groups
287 at week 8 ($p>0.05$). There was a significant increase in IGF-I in both male and female
288 training groups post-training ($p<0.05$), however there was no differences detected between
289 the groups ($p>0.05$, Table 1)

290

291 *Table 1: Baseline and post-training values for muscle-tendon complex properties and*
292 *circulating growth factors in each gender*

Measure	Males (n=8)			Females (n=8)		
	Baseline	Post-training	Change %	Baseline	Post-training	Change
pCSA (cm ²)	71±4	87±7	24±9**	40±3	52±5	30±10**
Strength (Nm)	223±25	254±10	26±18**	145±11	177±10	25±6**
T Vol (cm ³)	5.91±0.42	6.35±0.45	8±4*	4.10±0.24	4.38±0.32	6±2*
Mean PT K (N mm ⁻¹)	1132±104	1517±138	35±4**	619±72	887±108	46±11**
Mean PT E (GPa)	0.78±0.06	0.99±0.09	27±4*	0.42±0.04	0.60±0.08	46±16*
TGFβ-1 (pg nL ⁻¹)	5663±1524	4310±1248	-17±13	4716±1691	5276±2448	20±20
IGF-I (ng nL ⁻¹)	392±90	431±26	13±9*	380±24	460±42	23±9*

293 . * Significant difference compared to baseline ($p<0.05$) ** ($p<0.01$). Data are Mean \pm
294 S.E.M. pCSA; Vastus Lateralis physiological Cross-sectional area, T Vol; Patella Tendon
295 Volume, PT K; Patella Tendon Stiffness, PT E; Patella Tendon Modulus.

296

297

298 **Figure 1.** Relative changes in patella tendon stiffness (K) at each force level of the force-
299 elongation curve in males (black bars) and females (white bars) following training. *

300 Significant difference ($P<0.05$) between sex. Data are Mean \pm SEM.

301

302

303 *Associations between IGF-I and TGFβ-1 against MTC characteristics.*

304 There was a significant positive correlation between mean tendon stiffness and TGF β -1
 305 levels ($r=0.554$; $p=0.026$) in the pooled population at baseline. Baseline pooled (not sex
 306 specific) TGF β -1 levels also correlated with baseline stiffness at some (30, 50 and 60%
 307 MVC) but not all torque levels (Table 2). Pooled population week 8 TGF β -1 levels correlated
 308 with baseline tendon stiffness at 10% through to 80% MVC. Pooled population baseline IGF-
 309 I values correlated with baseline stiffness at high force levels (i.e. from 60-100% MVC) as
 310 well as correlating with average stiffness. At week 8 however, the correlations of IGF-I was
 311 in fact with lower force regions (i.e. 10-50% MVC).

312 *Table 2: Differential gender associations between circulating TBG- β , IGF-I and Tendon K.*
 313

%MVC		TGF β -1 at Wk0			TGF β -1 at Wk8			IGF-I at Wk0			IGF-I at Wk8		
		M	F	P	M	F	P	M	F	P	M	F	P
10%	Baseline K												
	Week 8 K												
	Δ K												
20%	Baseline K												
	Week 8 K												
	Δ K												
30%	Baseline K												
	Week 8 K												
	Δ K												
40%	Baseline K												
	Week 8 K												
	Δ K												
50%	Baseline K												
	Week 8 K												
	Δ K												
60%	Baseline K												
	Week 8 K												
	Δ K												
70%	Baseline K												
	Week 8 K												
	Δ K												
80%	Baseline K												
	Week 8 K												

	Δ K												
90%	Baseline K												
	Week 8 K												
	Δ K												
100%	Baseline K												
	Week 8 K												
	Δ K												
Average K	Baseline K												
	Week 8 K												
	Δ K												

314 Grey filled box denotes significant ($p < 0.05$) correlation between circulating hormone level
 315 and force level variable in pooled (P), male (M) and female (F) populations. Δ (delta) K,
 316 change in stiffness.

317 Our sex specific observations showed that in males, baseline TGF β -1 was associated with
 318 tendon stiffness at low forces (10-60% MVC). Post-training TGF β -1 levels correlated
 319 significantly with post-training tendon stiffness at all force levels >30%MVC. Interestingly,
 320 TGF β -1 levels post-training also correlated with baseline tendon stiffness, although at more
 321 moderate force levels (10-70%MVC). Whilst baseline IGF-I was not associated with tendon
 322 stiffness, at week 8, IGF-I levels correlated with week 8 stiffness at mid force levels (i.e. in
 323 the ranges of 20-60%MVC) as well as correlating with mean stiffness.

324 In contrast to the findings in males, females' baseline TGF β -1 did not correlate with stiffness
 325 at either baseline or post-training. Post-training TGF β -1 levels only correlated with post-
 326 training tendon stiffness at 80-90% MVC. The only apparent/statistically significant
 327 relationships observed in females were with post-training IGF-I levels which correlated with
 328 baseline tendon stiffness at 40-70%MVC and tendon stiffness at all force levels (10-100%
 329 MVC) post-training.

330

331 **Discussion:**

332 Our key current findings are 1) we are the first to demonstrate sex-specificity in the
333 overloading-induced adaptive nature of the mechanical properties of tendon in a young
334 population. 2) Although TGF β -1 and IGF-I levels may not reflect the entirety of adaptation
335 magnitude, they still appear to play an important role in chronic MTC characteristics. 3)
336 High-load, dynamic resistance training may not be optimal to enhance MTC characteristics in
337 females at higher portions of the tendon force-elongation curve.

338 Sex-related differences in the mechanical, structural and regulatory mechanisms in human
339 tendinous tissue have been identified previously (5, 7). Differences in acute tendon fractional
340 collagen synthesis rates (8, 9), amount of tendon dry mass per wet tendon weight (32),
341 mRNA levels of Type III collagen (10) have all been shown to vary between sexes. In
342 addition, proteomic work from Little et al. (33) demonstrated that alcohol dehydrogenase 1B,
343 MMP-3 and thrombospondin-1 (TSP-1) are enriched in female patella tendons compared to
344 male tendons, which suggests perhaps a reduced extra-cellular matrix regulatory or
345 remodelling function, and alteration of mechanical properties in females. This would tend to
346 suggest that, either at rest, or when provided with a similar physical stimulus to males, female
347 tendon does not respond similarly. As successive acute responses to physical stimuli combine
348 to produce the chronic adaptation, this leads to the possible scenario of a mal-adapted female
349 tendon (i.e. morphologically or mechanically) relative to male tendon following a period of
350 training.

351

352 *Morphology and Mechanical Properties*

353 In the current study, we found that patella tendon volume significantly increased in both
354 sexes by $8\pm 4\%$ and $6\pm 2\%$ in males and females respectively, with the small difference
355 between sexes not being statistically significant. There were also no differences in the
356 training-induced mean patella tendon stiffness change, between males and females. This is in

357 contrast to the findings of Onambele-Pearson and Pearson (12) and Seynnes et al. (13) who
358 found in older individuals (>70 years old), patella tendon stiffness changes in older males
359 were significantly greater than that seen in older females following resistance-type and alpine
360 skiing activities. What is interesting, in comparing the current investigation and the study of
361 Onambele-Pearson and Pearson (12), is that both report the 'character' or 'nature' of tendon
362 stiffness changes are inherently different between males and females following resistance
363 training regardless of age. In their study, Onambele-Pearson and Pearson describe a 'cut-off
364 point' of ~40%MVC, where below this juncture, females exhibited their greatest changes in
365 stiffness, and above it, males displayed their greater changes in stiffness. In a similar fashion,
366 we describe here for the first time in a young population, that at force levels of 10-20%MVC,
367 and at 90-100%MVC females have a significantly higher or lower RT-induced stiffness
368 change respectively than males, with a cut-off at ~55%MVC (see figure 2). Although not
369 immediately apparent why, one plausible explanation is that the tendon adapts to the loading
370 requirements it most frequently encounters, which in respect to males' tendons, is a lower
371 absolute load in females. Evident from the torque data in the current study, the mean torque
372 associated with the resistance training would have been much greater in males (post-training
373 MVCs were 254 ± 10 Nm vs. 177 ± 10 Nm in males and females respectively and were
374 significantly different at baseline), despite both groups training at the same relative load (but
375 distinct absolute loads).

376

377 **Figure 2.** Normalized change in tendon stiffness to the mean stiffness change following
378 training in males (black filled diamonds) and females (white filled squares) demonstrating an
379 improved stiffness at higher forces in males and a negative stiffness change at higher forces
380 in females.

381

382 *Resistance Training Program*

383

384 A further potential physiological mechanism for our observations is the nature of the
385 resistance training program. The exercises performed were dynamic (apart from one
386 isometric), and isotonic in nature. Adaptations to eccentric training, such as microcirculatory
387 factors and pain reduction, has been shown to be sex-specific in a cohort with Achilles
388 tendinopathy, with males again demonstrating an improved responsiveness (34).
389 Furthermore, during maximal eccentric exercise between 20-90° knee extension, we
390 previously (7) showed that female patella tendon displayed reduced stiffness compared to
391 males, and attributed a large portion of the reduced fascicular lengthening seen in females
392 compared to males to this observation. A subsequent study from our group (35) also showed
393 that following the same exercise protocol, males displayed a significantly greater magnitude
394 of muscle damage. This demonstrates that the sex-specific response and adaptations to
395 variables associated with manipulating a resistance training program have yet to be
396 elucidated, and await further study. Therefore, the results of the current study raises the
397 following question: Is dynamic, heavy-load resistance training (currently the most
398 conventional and popular form), the best training method for females routinely operating at
399 the higher force levels of the tendon force-elongation curve, where adaptations to this type of
400 training are minimised relative to adaptations on the subsequent lower portions of the tendon
401 Force-Elongation curve?

402 *Circulating IGF-I/ TGFβ-1*

403

404 A further novel aspect of the current investigation was to ascertain the changes to circulating
405 growth factors related to tendon and ECM responses/adaptation. *In vitro* studies have
406 demonstrated the potency of TGFβ-1-mediated effects on collagen, and its relationship to
407 magnitude of mechanical strain (14, 15). Despite the vast array of data from *in vitro* studies
408 outlining the roles of TGFβ-1 in tendon and ECM maintenance/ repair, data from *in vivo*

409 human exercise studies is scarce. What is also surprising is that to date, only one study had
410 previously described the effect of resistance training as opposed to endurance kicking-type
411 exercise, on TGF β -1 and tendon mechanical properties, despite resistance training being a
412 more potent mechanical stimulus for tendon adaptation. We have also previously shown in a
413 young population (31), that resistance training did not result in chronically elevated TGF β -1
414 levels following 8 weeks of heavy resistance training with varying levels of strain. This was
415 also the case in the current study, where there were no significant changes in either males or
416 females following resistance training, despite significant improvements in tendon mechanical
417 properties. Although a ~30% post-exercise increase in circulating TGF β -1 associated with
418 increased local Type I collagen synthesis and peri-tendinous TGF β -1 levels has been
419 documented (22), it may be that TGF β -1 does not remain chronically elevated to maintain a
420 healthy (non-fibrotic) connective tissue profile. Thus, within the confines of the current
421 study's experimental design, measurement of pre-and post-8 weeks of resistance training may
422 not have been facilitative in uncovering TGF β -1's mechanistic role. Despite this, we have
423 shown a strong, positive correlation between baseline TGF β -1 levels and tendon stiffness.
424 This would make sense, from the point that a natural higher physiological level of TGF β -1
425 could produce and preserve a stiffer MTC. Previous research has shown, lower levels of
426 TGF β -1 and dysregulation of the TGF- β axis are present in diseased compared to healthy
427 tendons (36). It should nonetheless be noted that measuring TGF β -1 in blood is a complex
428 issue, with many large variations measured between studies. However, in a young, healthy
429 population, such as in the current study, there have been shown to be no differences between
430 male and females in circulating TGF β -1 levels (19, 20). Furthermore, our reported circulating
431 TGF β -1 levels are consistent with previously published data in a review using the same
432 ELISA kit (R&D systems) and a robust TGF β -1 sampling methodology (20).

433 IGF-I levels increased significantly as a result of heavy resistance training in both sexes.
434 Similar observations have also been made, with peritendinous levels of IGF-I being
435 significantly elevated at 3 hours post-RT in both males and females, but in females only,
436 remaining elevated at 4 hours post RT (18). In a patella tendon defect model in rabbits, direct
437 administration of IGF-I and TGF β -1 together significantly improved the mechanical
438 properties of tendon such as force at failure, ultimate stress and stiffness (17). Results from
439 the studies of Doessing and co-workers (37) and Nielson et al. (16) demonstrate that IGF-I,
440 and the regulatory function of the growth hormone/ IGF-I axis, are important factors for the
441 matrix collagen fractional synthetic rate, expression of Type I collagen and tendon function.
442 Circulating levels of IGF-I do not allow distinction between effects on muscle and/or tendon.
443 In the current study, males and females showed very similar relative changes in IGF-I,
444 muscle size, torque, tendon volume and tendon mechanical properties. IGF-I thus may have
445 played a role in the adaptive process, with the work of Doessing et al. (37) suggesting that
446 IGF-I may play a more prominent role in tendinous as opposed to muscular adaptation.

447 *Practical Application*

448 It has been suggested that young, exercising females are possibly at more risk of tendon
449 injury than males (4). The practical implications of the current study are that females
450 operating toward the maximal end of the MVC spectrum, may experience a relatively
451 reduced enhancement of tendon stiffness following RT. A sex-specific electromechanical
452 delay has been noted previously (38), with females showing an increased delay compared to
453 males. In parallel, we have also previously demonstrated that during maximal eccentric
454 contractions (7), there are sex differences in absolute patella tendon stiffness, which in turn
455 modulated *Vastus Lateralis* fascicle lengthening, affecting force production. These above
456 facts compound the evidence and necessity to consider sex difference in resistance training
457 applications. Therefore, female athletes involved in sprint/power activities may find that

458 transfer of contractile force to bone during a high-force effort may be compromised in terms
459 of amount of force and/ or rate of force development due to sub-optimal changes in stiffness,
460 or indeed reduced force development due to modulation of the fascicular shortening.
461 Therefore, future studies may wish to focus on elucidating methods to increase stiffness at
462 higher MVC forces in young, female populations.

463 **Conclusion:**

464 In conclusion, we have demonstrated that both males and females display the same relative
465 adaptability in terms of enhancing muscle-tendon morphology and function following
466 resistance training. However, the nature of these adaptations have implications for muscle-
467 tendon function during different tasks for each sex. Finally, for females, high-load dynamic
468 resistance training may not be optimal for enhancing MTC function at high force outputs.

469

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473

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