

## **Comparison of Three Gaze Position Calibration Techniques in First Purkinje-Image Based Eye Trackers**

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**Significance:** This study highlights potential differences that can arise in gaze position estimates from 1st Purkinje image-based eye trackers based on how individual Hirschberg ratios are calculated.

**Purpose:** To evaluate the accuracy and repeatability of eccentric-viewing, prism-based and theoretical techniques that are routinely used to calibrate Hirschberg Ratio (HR) in 1<sup>st</sup> Purkinje image-based eye trackers.

**Methods:** Hirschberg ratios of 28 UK participants (18-40 years) were obtained using the PlusOptix PowerRef3 photorefractor and eye tracker. In the gold-standard eccentric viewing technique, participants viewed eccentric targets ( $\pm 12^\circ$ ,  $4^\circ$  steps) at 2m. In the prism-based technique, 4-16 $\Delta$ D base-out and base-in prisms were placed in 4 $\Delta$ D steps before an eye occluded with an infrared filter; the fellow eye fixated a target at 1m. Each participant's HR was calculated as the slope of the linear regression of the shift in Purkinje image, relative to the pupil centre, for each target eccentricity or induced prism power. Theoretical HR was calculated from the participant's corneal curvature and anterior chamber depth measures. Data collection was repeated on another visit using all three techniques to assess repeatability. Data were also obtained from an Indian cohort (n=30, 18-40 years) using similar protocols.

**Results:** HR ranged from 10.61-14.63 $^\circ$ /mm (median: 11.90 $^\circ$ /mm) in the eccentric viewing technique. The prism-based and theoretical techniques demonstrated inaccuracies of 12% and 4% relative to the eccentric viewing technique. The 95% limits of agreement of intra-subject variability ranged from  $\pm 2.00^\circ$ /mm,  $\pm 0.40^\circ$ /mm, and  $\pm 0.30^\circ$ /mm for the prism-based, eccentric viewing and theoretical techniques ( $P > .05$ ). Intraclass correlation coefficients (95%CI) were 0.99 (0.98-1.00) for eccentric, 0.99 (0.99-1.00) for theoretical and 0.88 (0.74-0.94) for prism-based techniques. Similar results were found for the Indian cohort.

**Conclusion:** The prism-based and theoretical techniques both demonstrated relative inaccuracies in measures of Hirschberg ratio, compared to the eccentric viewing technique. The prism-based technique exhibited the poorest repeatability.

**Keywords:** Anterior chamber depth, corneal curvature, eye tracker, gaze position, Hirschberg ratio, Purkinje-image, repeatability, variability

1 Video-based eye trackers are increasingly used in research laboratories and clinical settings to  
2 obtain quantitative estimates of gaze position.<sup>1-3</sup> This is a valuable measure in studies investigating  
3 the biology of eye movements or those that use movements as an objective biomarker for assessing  
4 cognition<sup>4, 5</sup> or tracking disease progression.<sup>6</sup> These trackers use specific landmarks (e.g. 1<sup>st</sup> Purkinje  
5 image, limbus, pupil margin and blood vessel configuration) to rapidly and non-invasively track gaze  
6 position.<sup>7, 8</sup> Of the variety of eye trackers commercially available, those using the relative location of  
7 the 1<sup>st</sup> Purkinje image and entrance pupil center (i.e. virtual image of the anatomical pupil as seen  
8 through the cornea and anterior chamber<sup>9</sup>) as landmarks are of specific interest to the present study.  
9 A proportionality constant or calibration factor – the Hirschberg ratio is used in these trackers to  
10 directly convert the millimetre separation between the Purkinje image and pupil center into angular  
11 units of gaze position in degrees or prism dioptres ( $\Delta$ D).<sup>10, 11</sup> Accuracy of gaze position estimates  
12 obtained by these trackers, relative to a gold-standard, depends on the accuracy of this calibration  
13 factor and on the angle kappa (i.e. the angle between the pupillary axis and visual axis).<sup>12,3</sup> Previous  
14 studies have reported a large inter-subject variability in Hirschberg ratio between 7 to 16°/mm (12  
15 to 28  $\Delta$ D/mm),<sup>3, 9, 12, 13</sup> and consequently, using a population-average Hirschberg ratio as the  
16 calibration factor (e.g. 11.8°/mm as used by the PlusOptix PowerRef3 device used in this study<sup>12</sup>) could  
17 result in inaccurate estimation of eye position. Using an individual’s Hirschberg ratio as the calibration  
18 factor therefore enhances the accuracy of gaze position estimates determined by these eye trackers.<sup>12</sup>

19

20 Three techniques have been described in the literature to measure the individual Hirschberg  
21 ratio.<sup>12-14</sup> In the eccentric viewing technique, Hirschberg ratio is measured by asking participants to  
22 fixate on targets placed before them at known angular eccentricities and measuring the separation  
23 between the Purkinje image and pupil center for each of these positions using the eye tracker’s high-  
24 resolution camera.<sup>12</sup> The reciprocal of the slope of a linear regression fit of the measured separation  
25 between Purkinje image and pupil center against the corresponding target eccentricity gives the  
26 Hirschberg ratio in degrees or prism dioptres per millimetre.<sup>7, 11, 15</sup> In the theoretical technique,  
27 Hirschberg ratio is derived from biometric measures of the eye’s corneal curvature and anterior  
28 chamber depth using basic geometric formulae derived by Brodie.<sup>7, 12</sup> Finally, the prism-based  
29 technique involves the use of prism of known base powers to change the separation between Purkinje  
30 image and pupil center and derives Hirschberg ratio by calculating the reciprocal of the slope of a  
31 linear regression fit of the measured separation between these landmarks against a range of induced  
32 prism power.<sup>14, 16</sup> The fundamental characteristics, and practical advantages and disadvantages of all  
33 three techniques are presented in Table 1.

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35 -----

36 Table 1 about here

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38

39           The utility of a given technique for measuring Hirschberg ratio in a clinical or research setting  
40 depends on how successfully the technique can be implemented, how accurate the estimates of eye  
41 positions are using this technique and how variable are the eye position estimates over repeat  
42 measurements using this technique for the subject group. While some studies have investigated the  
43 accuracy and repeatability of the eccentric viewing and the theoretical techniques and the agreement  
44 between them,<sup>3, 11, 12, 17</sup> there is no such information available for the prism-based technique. There  
45 are also no published data describing how the three techniques compare with each other. Therefore,  
46 the overall aim of this study was to determine the accuracy, repeatability and agreement of Hirschberg  
47 ratios obtained using each one of these three techniques.

48

#### 49 **Materials and methods**

50           Adult subjects aged 18 – 40 years were recruited from staff and students of Ulster University  
51 (UU), Coleraine, Northern Ireland, UK (n=28). All subjects that participated in the study had a  
52 presenting distance visual acuity of 20/20 or better and were either emmetropic (-0.25D to +1.00D  
53 spherical equivalent refractive error) or myopic (-0.50 to -6.00D spherical equivalent refractive error)  
54 for the fixated eye (Table 2). Subjects were required to have refractive errors limited to <1.00D  
55 anisometropia, and no more than 0.75DC of astigmatism. Subjects were corrected using soft contact  
56 lenses as measurement of lens calibration was also being undertaken as a part of a different study  
57 (Table 2). These soft contact lenses conformed to the shape of the cornea and produced minimal  
58 movement during measurement. None of the subjects presented with any ocular pathology or  
59 binocular vision anomaly. Subjects with amblyopia, pupil diameters <3.00mm (below the operational  
60 range of the device) in a dimly lighted room, who could not maintain steady fixation or had an  
61 excessive blink rate were excluded.

62

63           Data from a parallel study with small variations in experimental protocol and participant  
64 cohort were collected from the Brien Holden Institute of Optometry and Vision Sciences, LV Prasad  
65 Eye Institute (LVPEI), Hyderabad, India to determine the generality of the study outcomes in the UU  
66 cohort. Table 2 summarises the participant characteristics in both cohorts. The study was conducted  
67 in accordance with the tenets of the Declaration of Helsinki and commenced after approval by the  
68 local Research Ethics Committee at UU and the Institutional Review Board at LVPEI.

69 Gaze position data were obtained using the PowerRef 3™ (Nuremberg, Germany) at a sampling  
70 frequency of 50Hz for the prism-based calibration and the eccentric viewing calibration techniques.  
71 The device is designed to capture dynamic measurements of the eye’s refractive power at the pupil  
72 plane using eccentric photorefractive technique.<sup>18</sup> To do so, the device is fitted with an array of  
73 infrared light emitting diodes adjacent to the camera aperture, and this arrangement produces a crisp  
74 1<sup>st</sup> Purkinje image, which can be compared to the position of the pupil center in the vertical and  
75 horizontal meridian to determine respective gaze positions. Additional technical information about  
76 the photorefractor used in this study can be found at [https://plusoptix.com/images/support-](https://plusoptix.com/images/support-downloads/powerref3-specifications-usa.pdf)  
77 [downloads/powerref3-specifications-usa.pdf](https://plusoptix.com/images/support-downloads/powerref3-specifications-usa.pdf). The use of different versions of eccentric  
78 photorefractors for eye movement research has been previously reported,<sup>12, 14, 16, 19</sup> and more research  
79 is being conducted with these instruments. Therefore, this study used the PowerRef 3™ as a model  
80 instrument of 1<sup>st</sup>Purkinje image-based eye trackers for investigating the repeatability of three gaze  
81 position calibration techniques, using eccentric viewing technique as the reference gold-standard. The  
82 set-up for these techniques is described below for the UU data collection. The LVPEI data collection is  
83 broadly similar, but Table 2 lists the variations between the two study sites.

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86 Figure 1 about here  
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88  
89 Eccentric viewing technique

90 In the eccentric viewing technique, subjects fixated with their left eye on a series of Maltese  
91 cross targets arranged linearly at 2m while the right eye was occluded. The entire target array, from  
92 left to right, produced eccentricity of  $\pm 12^\circ$ , with each target separated from the adjacent by  $4^\circ$ . These  
93 target eccentricities were all within the  $\pm 25^\circ$  range described by Brodie, where the millimetre  
94 separation between the Purkinje image and pupil center varies linearly with angular eccentricity.<sup>13</sup>  
95 Beyond this range, the separation between these two landmarks varies in a sinusoidal manner with  
96 angular eccentricity.<sup>13</sup>

97  
98 Prism-based technique

99 In the prism-based calibration technique, the dominant eye fixated on a Maltese cross target  
100 at 1m while the fellow non-dominant eye was occluded using an Optcast long pass infrared  
101 transmitting filter (Edmund Optics™, NT43-954). This filter blocks virtually all the visible wavelengths  
102 while allowing infrared light from the camera to pass through it. Prisms from 0Δ to 16Δ in 4Δ steps

103 were held before the occluded eye in a base-in and base-out sequence, at a vertex distance of 10–14  
104 mm for at least four seconds each. This experimental set-up helped to eliminate any compensatory  
105 vergence eye movements from the fellow eye that might contaminate the eye position calibration  
106 results. Prism powers were converted into degrees using the formula: where degrees = arctan (prism  
107 dioptres/100). The prism powers used here thus corresponded to target eccentricities of  $\pm 9.09^\circ$ , in  
108 steps of  $2.29^\circ$ .

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110 -----

111 Table 2 about here

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114 Gaze position calibration measurements in both prism-based and eccentric viewing  
115 techniques were made in a dimly lit room. Data analysis was performed using custom written software  
116 in Matlab®. Raw PowerRef 3™ data were processed, removing blinks and extraneous data outside of  
117 the instrument working range. Eye movement data were plotted against time and scrutinised for a  
118 section of stable gaze, and two seconds worth of data (~100 samples) from each prism power or target  
119 position was selected and averaged.<sup>14, 16</sup> These averaged gaze positions were plotted against the  
120 corresponding prism power and target eccentricity in prism-based and eccentric viewing techniques,  
121 respectively. Linear regression analysis was performed to obtain the eye position calibration slope.  
122 The slope of this linear regression equation provided an estimate of the subject's Hirschberg ratio. The  
123 calibration slope obtained from these two techniques is a unitless quantity describing the change in  
124 eye position recorded by the PowerRef 3™ for a unit change in target eccentricity or prism power. The  
125 actual Hirschberg ratio of the individual will be equal to that used by the PowerRef 3™ divided by the  
126 calibration slope of that individual obtained using these techniques. In other words, an eye position  
127 calibration slope that is equal to unity indicates an Hirschberg ratio of  $11.8^\circ/\text{mm}$  (i.e. equal to the  
128 population average value used by the machine). Eye position calibration slopes greater than unity  
129 correspond to Hirschberg ratios  $<11.8^\circ/\text{mm}$  (smaller than population average value) while calibration  
130 slopes smaller than unity correspond to Hirschberg ratios  $>11.8^\circ/\text{mm}$  (larger than population average  
131 value).

132  
133 Theoretical technique

134 The theoretical calibration technique was based on the geometric optics model described by  
135 Brodie, which posits that the Hirschberg ratio of the individual varies with their anterior corneal  
136 curvature and the anterior chamber depth.<sup>7</sup> The procedure of obtaining Hirschberg ratio using the

137 theoretical technique is explained in detail by Jagini et al.<sup>12</sup> Briefly, the average of three measurements  
138 of horizontal corneal curvature and anterior chamber depth of each subject was obtained using the  
139 Zeiss IOL Master™. These values were used to theoretically predict the Hirschberg ratio using the  
140 regression equation previously described by Jagini et al.<sup>12</sup> All theoretical calculations were performed  
141 using custom software in Matlab®. Data from the left eye are presented for the theoretical technique  
142 to allow for comparison with the other techniques.

143

144 Repeatability of Hirschberg ratio obtained with the three techniques was assessed by repeating each  
145 technique for a second time within a week of the first measurement.

146

### 147 **Data analysis**

148 Representative eye position raw data and the linear regression fits that were derived from  
149 these data for the eccentric viewing and the prism-based techniques are shown in Figure 1. There  
150 were excellent linear regression fits for both prism-based and eccentric viewing calibration techniques  
151 with  $r^2$  value  $\geq 0.90$  in all subjects (consistent with previous work), and this was a criterion for inclusion  
152 of data.<sup>12</sup> The Kolmogorov-Smirnov test indicated that the corneal curvature, anterior chamber depth  
153 and Hirschberg ratio calculated from the slopes were not normally distributed and, therefore, non-  
154 parametric statistics described the data. One-way ANOVA was used to assess the mean difference  
155 between the three techniques and the post-hoc Scheffe test was used to determine differences  
156 between the individual groups while the paired t-test was used to assess mean differences between  
157 baseline and repeat measures. The intraclass correlation coefficient (ICC, two-way mixed effects) was  
158 used to assess absolute agreement between measures. Results of intraclass correlation test were  
159 considered excellent, good, moderate, and poor if  $>0.90$ ,  $0.75$  to  $0.90$ ,  $0.50$  to  $0.75$ , and  $<0.50$ ,  
160 respectively.<sup>20</sup> Linear regression analysis was used to determine range effects in Hirschberg ratio.  
161 Significance was determined as  $P < .05$ .

162

### 163 **Results**

164 Data collection was successful in all 28 subjects recruited at UU and in all 30 subjects recruited  
165 at LVPEI. The data from the UU cohort will be described first followed by a description of the data in  
166 the LVPEI cohort. Given the differences in experimental protocols employed in the two study  
167 locations, albeit minor, the two datasets are considered as stand-alone entities and no explicit  
168 comparison is made between the two datasets. Only general judgments about the accuracy and  
169 repeatability of the Hirschberg ratio measurements from the three protocols are made from the data  
170 obtained from the two study locations.

171 Data from the UU cohort

172 The baseline regression slopes ranged from 0.81 to 1.11 [median (25<sup>th</sup>-75<sup>th</sup>interquartile range;  
173 IQR) =0.99 (0.91–1.03)] for the eccentric viewing technique, and 0.70 to 1.03 [0.89 (0.79-0.93)] for the  
174 prism-based technique (Table 3). The Hirschberg ratios calculated from these slopes ranged from  
175 10.61 to 14.63°/mm [11.90°/mm (11.44–12.97°/mm)] for the eccentric viewing technique and 11.47  
176 to 16.93 °/mm [13.30°/mm (12.74–15.06°/mm)] for the prism-based technique Table 3 and Figure 2A).  
177 Baseline corneal curvatures and anterior chamber depth results are presented in Figure 2B. These  
178 translated into theoretically derived Hirschberg ratios ranging from 9.84 to 13.44°/mm [11.43°/mm  
179 (10.55–11.96°/mm)] (Table 3).

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181 -----

182 Table 3 and Figure 2 about here

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185 Results of one-way ANOVA test showed an overall statistically significant difference (signed  
186 difference) between the mean Hirschberg ratio of all three techniques ( $F_{(2,81)} = 31.24, P<.0001$ ). Post-  
187 hoc test using Scheffe method showed statistically significant differences between the mean  
188 Hirschberg ratio of the prism-based and eccentric viewing techniques (-1.63 °/mm,  $P<.001$ ), between  
189 the prism-based and theoretical techniques (-2.54 °/mm,  $P<.001$ ) and between the eccentric viewing  
190 and theoretical techniques (-0.91 °/mm,  $P=.024$ ), Table 4 (signed difference). However, to determine  
191 if the difference between the techniques varied as a function of calculated Hirschberg ratios, the mean  
192 absolute difference between the Hirschberg ratios was computed and presented with the mean  
193 signed difference (Table 4). The Bland-Altman type plots of the absolute difference between  
194 techniques indicated that there was systematic bias in the Hirschberg ratios obtained from one  
195 technique, relative to the other (Figures 3A – C). Linear regression analyses were performed on the  
196 absolute difference to determine the effect of Hirschberg ratio size on the mean difference. Results  
197 of this analysis indicated that the slopes were significantly different from zero between the prism-  
198 based and eccentric viewing techniques (Linear regression equation:  $Y= -4.18 + 0.46X$  ( $X=$  inter-  
199 technique average Hirschberg ratio):  $F_{(1,26)}=7.52, P=.01$ ), and between the prism-based and theoretical  
200 techniques (Linear regression equation:  $Y= -5.51 + 0.64X$ :  $F_{(1,26)}=6.98, P=.01$ , (Figures 3A and B show  
201 this effect). However, there was no such Hirschberg ratio range effects on the mean difference  
202 between the eccentric and theoretical techniques (Linear regression equation:  $Y= -0.80 + 0.15X$ :  $F_{(1,26)}$   
203  $= 0.34, P=.57$ ), (Figure 3C).

204 To determine the intra-subject variability of the three Hirschberg ratio techniques, each  
205 technique was repeated for a second time within a week of the baseline measurement reported  
206 (Figure 4A – C). The mean difference (95% LOA) in Hirschberg ratio between the first and second  
207 measurements were 0.05°/mm (95% LOA: -0.30 to 0.40°/mm) for the eccentric viewing technique  
208 (Figure 4A) and 0.09°/mm (95% LOA: -1.91 to 2.08°/mm) for the prism-based technique (Figure 4B).  
209 Median repeat corneal curvature and anterior chamber depth measures for calculating Hirschberg  
210 ratio using the theoretical technique was 7.91 (7.80 – 8.29mm) and 3.54 (3.28 – 3.74), respectively.  
211 These translated into median Hirschberg ratio of 11.45°/mm (10.45 – 11.93°/mm). The mean intra-  
212 subject variability of the theoretically derived Hirschberg ratio was therefore 0.04°/mm [paired t-test  
213 (95% LOA: -0.20 to 0.28°/mm)] (Figure 4C). The mean difference between the first and repeat  
214 measures of Hirschberg ratio for all three techniques was not significantly different (all  $P > .05$ ).  
215 Moreover, results of intraclass correlation test revealed excellent repeatability in the eccentric  
216 viewing and theoretical techniques [0.99(95% CI: 0.98-0.997),  $P < .001$ , and 0.99 (95% CI: 0.99-0.998),  
217  $P < .001$ , for the eccentric viewing and theoretical techniques respectively]. In the prism-based  
218 technique, there was a good agreement between the first and repeat measures 0.88(95% CI: 0.74-  
219 0.944),  $P < .001$ ) (Table 3).

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222 Figures 3 and 4 about here

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224

225 Data from the LVPEI cohort

226 The baseline regression slopes ranged from 0.79 to 1.24 [median (25<sup>th</sup>-75<sup>th</sup>IQR) = 1.04 (0.98–  
227 1.09)] and 0.76 to 1.12 [0.97 (0.91–1.03)] in the eccentric viewing and prism-based techniques,  
228 respectively (Table 3). The Hirschberg ratios derived from these regression slopes are shown in Table  
229 3 and Figure 5A. The baseline corneal curvatures and anterior chamber depth results are presented in  
230 Figure 5B and the theoretically derived Hirschberg ratios from these values are shown in Table 3.  
231 Results of one-way ANOVA test showed an overall statistically significant difference (signed  
232 difference) between the mean Hirschberg ratio of all three techniques ( $F_{(2,87)} = 4.25$ ,  $P = .01$ ). Post-hoc  
233 test using Scheffe method showed significant differences between the mean Hirschberg ratio of the  
234 prism-based and eccentric viewing techniques (-0.77 °/mm,  $P = .03$ ). However, there was no statistically  
235 significant difference between the prism-based and theoretical techniques (-0.67 °/mm,  $P = .06$ ) and  
236 between the eccentric viewing and theoretical techniques (0.10 °/mm,  $P = .93$ ). As before, results of  
237 the absolute difference are presented in Bland Altman plots in Figure 6A-C, see also Table 4. There

238 were no Hirschberg ratio range effects on the mean absolute difference between the prism-based and  
239 eccentric viewing techniques (Linear regression equation:  $Y = -2.13 + 0.27X$  ( $X =$  inter-technique average  
240 Hirschberg ratio):  $F_{(1,28)} = 2.79$ ,  $P = .11$ ), and between the prism-based and theoretical techniques (Linear  
241 regression equation:  $Y = -1.52 + 0.20X$ :  $F_{(1,28)} = 3.71$ ,  $P = .06$ ) (Figure 6A&B). However, range effect was  
242 observed on the mean difference between the eccentric viewing and theoretical techniques (Linear  
243 regression equation:  $Y = -2.14 + 0.23X$ :  $F_{(1,28)} = 4.62$ ,  $P = .04$ ) (Figure 6C).

244  
245 Repeatability of the Hirschberg ratio estimate was available only for the prism-based  
246 technique in the LVPEI cohort and this data showed a mean difference (95% LOA) in Hirschberg ratio of  
247  $0.08^\circ/\text{mm}$  (95% LOA:  $-1.7$  to  $1.9^\circ/\text{mm}$ ) ( $P = .63$ ) (Figure 6D), and the intraclass correlation test of  
248 absolute agreement between the first and second measures showed good agreement between the  
249 two [ $0.83$ (95%CI:  $0.64$ - $0.92$ ),  $P < .001$ ] (see Table 3).

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251 -----

252 Figure 6 about here

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254  
255 **Discussion**

256 The essence of calibrating an individual's Hirschberg ratio in 1<sup>st</sup> Purkinje image-based eye  
257 trackers is to reduce the errors in gaze position estimates that may arise while using the population-  
258 average Hirschberg ratio.<sup>3, 9, 12</sup> This problem is of real concern to commonly used eye trackers given  
259 the large inter-subject variability in Hirschberg ratio that has been reported in the literature.<sup>3, 9, 11, 12</sup>  
260 Following the decision to use the subject's own Hirschberg ratio to calibrate the eye tracker for  
261 improved accuracy, a second challenge is to determine which calibration technique is to be adopted  
262 for this purpose. The performances of three such techniques that have been used previously in the  
263 literature –eccentric viewing, prism-based and theoretical – were tested in the present study. To  
264 determine the accuracy of a given calibration technique, the values obtained by this technique need  
265 to be compared against a “gold-standard” measure. For the present analysis, the eccentric viewing  
266 technique is considered as the “gold-standard” technique simply because of its traditional use for  
267 calibrating the Hirschberg ratio in most 1<sup>st</sup> PI-based eye trackers.<sup>3, 21</sup> This technique has also become  
268 a “legacy technique” from which the population-average Hirschberg ratio has been derived in previous  
269 studies.<sup>3, 21</sup> Moreover, this technique uses angles anchored in space, and it is based on actual eye  
270 rotations, thus requires few assumptions to be made for deriving the Hirschberg ratio.

271 Compared to the eccentric viewing technique, the prism-based and theoretical techniques  
272 both demonstrated relative inaccuracies of 12% and 4% respectively in the UU cohort when the  
273 median values were compared [see Table 3 for median values:  $(100 - (13.30 \div 11.90) \times 100) = 12\%$ ), and  
274  $(100 - (11.43 \div 11.90) \times 100) = 4\%$ ]]. In the LVPEI cohort, similar inaccuracies of 7% and 3% were recorded  
275 in the prism-based and theoretical techniques respectively. At individual level, these inaccuracies  
276 ranged from 6% of underestimation of the Hirschberg ratio to 33% of overestimation in the theoretical  
277 technique, and 20% underestimation to 37% overestimation in the prism-based technique in the UU  
278 cohort; and 19% underestimation to 13% overestimation, and 23% underestimation to 29%  
279 overestimation in the theoretical and prism-based techniques respectively in the LVPEI cohorts.

280 The present study also demonstrated the over-estimation of Hirschberg ratio by the prism-  
281 based technique, relative to both the eccentric-viewing and theoretical techniques (Figure 3A and B).  
282 This was particularly significant in the UU cohort, although there were range effects in the bias towards  
283 the prism-based technique and with the difference between techniques appearing to increase with an  
284 increase in the size of the Hirschberg ratio (Figure 3A and B). However, there was no such range effect  
285 between the eccentric viewing and theoretical techniques, and the mean difference between the two  
286 was closer to zero compared to the mean differences when the prism-based technique is considered.  
287

288 In addition to accuracy, the calibration technique's repeatability also needs to be assessed to  
289 determine its usefulness in estimating the individual Hirschberg ratio. The theoretical technique  
290 demonstrated the least intra-subject variability as the Hirschberg ratio obtained with this technique  
291 was repeatable to within  $\pm 0.30^\circ/\text{mm}$  95% LOA in a subject, less than the  $0.50^\circ/\text{mm}$  95% LOA previously  
292 reported by Jagini et al.<sup>12</sup> This may be attributed to the more consistent, repeatable measures of  
293 corneal curvature and anterior chamber depth ( $\sim 0.01\text{mm}$  for both measures in this study, less than  
294 the  $0.08\text{mm}$  reported previously<sup>12, 22, 23</sup>) available in the present study. The Hirschberg ratio obtained  
295 using the eccentric viewing technique was repeatable to within  $\pm 0.40^\circ/\text{mm}$  95% LOA in individual  
296 subjects; slightly less repeatable than the theoretical technique, but more repeatable than the prism-  
297 based technique. Furthermore, there was improved intra-subject repeatability in the eccentric  
298 viewing technique in this study than previously reported (1.5 to 3.0 degrees/mm).<sup>21, 24</sup> The use of  
299 different fixation targets in the present study compared to previous work could explain the differences  
300 in the intra-subject repeatability reported as fixation target characteristics are known to affect the  
301 stability of eye movements.<sup>25</sup> Perhaps the use of Maltese cross fixation target in this study minimized  
302 micro-eye movements, thereby contributing to enhanced repeatability. The highest intra-subject  
303 variability in Hirschberg ratio, with the lowest intraclass correlation coefficient was observed in the  
304 prism-based technique. The Hirschberg ratio measured in the prism-based technique was repeatable

305 to within  $\pm 2.0^\circ/\text{mm}$  at UU and  $\pm 1.9^\circ/\text{mm}$  at LVPEI. There are no previously published data with which  
306 to compare these findings, but when compared with the other two techniques in this study, the  
307 variability exhibited by the prism-based technique is high (Figure 4, panel B and Figure 6, panel D).  
308 Moreover, the lowest intraclass correlation coefficient was recorded in the prism-based technique  
309 demonstrating least agreement between the baseline and repeat measures. It is possible that the high  
310 variability in Hirschberg ratio exhibited in the prism-based technique is inherent when using prisms  
311 for calibration. Variability in Purkinje image displacements which can arise from minimal variance in  
312 orientation and/or placement of the prisms before the infrared-occluded eye during repeat  
313 measurements will influence the results.<sup>26</sup> Furthermore, variability in a subject's phoria adaptation at  
314 different measurement times,<sup>27</sup> could lead to the high variability observed with the prism-based  
315 technique. Finally, potential conflicts in fixation between the target presented to the non-occluded  
316 eye and the image of the infrared LED's in the occluded eye could lead to additional variability in this  
317 technique.

318

319 Another way to quantify the precision of a technique, is to compare the intra-subject and  
320 inter-subject variability of the technique. If the magnitude of intra-subject variability equals the inter-  
321 subject variability produced by the technique, then its usefulness for calibration could be questioned.  
322 In the case of theoretical technique, the intra-subject variability was 13% relative to the inter-subject  
323 variability [see Table 3 UU section, for a  $-0.20$  to  $0.28^\circ/\text{mm}$  of intra-subject variability, expressed as  
324 percentage of its inter-subject variability ( $9.84$  to  $13.44^\circ/\text{mm}$ ):  $(0.48 \div 3.6 \times 100) = 13\%$ ]. Similarly, the  
325 eccentric viewing technique exhibited 17% variability of the inter-subject value. However, the prism-  
326 based technique exhibited 73% variability in both cohorts relative to the inter-subject variability [e.g.  
327 for a  $-1.91$  to  $2.08^\circ/\text{mm}$  in the UU cohort, expressed as percentage of its inter-subject variability ( $11.47$   
328 to  $16.93^\circ/\text{mm}$ ):  $(3.99 \div 5.46 \times 100) = 73\%$ ]. From these data, it is evident that the prism-based  
329 technique exhibited the greatest variability relative to the other two.

330

331 In the present study, data from two laboratories that evaluated three gaze position calibration  
332 techniques using similar (but not identical) protocols are presented together in one publication. The  
333 differences in protocols include: 1) the assessment of agreement between the eccentric viewing and  
334 prism-based techniques in the UU data is limited by the fact that the non-dominant eye was used in  
335 the prism-based technique, whereas the left eye was used in eccentric viewing technique (Table 2).  
336 However, subjects were all binocularly normal, and wore optical correction during assessments, which  
337 would have minimized any possible effects. Additionally, there was a high intraclass correlation  
338 between the two ocular biometric measures of the two eyes [ $0.99$ (95% CI:  $0.98$ - $0.99$ ),  $P < .001$  and

339 0.99(0.97-0.99),  $P < .001$ ] for the corneal curvature and anterior chamber depth, respectively. With this  
340 very high level of agreement, the Hirschberg ratio of a subject would not have been significantly  
341 different regardless of which eye was used in the prism-based technique; 2) subjects in the LVPEI  
342 cohort includes myopes who were not optically corrected during the data collection process while  
343 those at UU were corrected with soft contact lenses (Table 2). While this could affect accurate fixation  
344 of targets in theory, it has been reported that blur from moderate levels of uncorrected refractive  
345 errors has minimal impact on fixation accuracy, and rather that fixation target characteristics are  
346 critical in determining accuracy and stability<sup>28,29</sup>; 3) the two study centers used different technologies  
347 to obtain measures of corneal curvature and anterior chamber depth in subjects (Table 2). Although  
348 the individual instruments have been shown to produce accurate and repeatable measures of the two  
349 ocular biometric parameters,<sup>22, 30-32</sup> we are unable report on the agreement between these  
350 instruments, even though they produce overlapping results. However, despite these differences in  
351 protocols, there was a general similarity in the results in that the corneal curvature and anterior  
352 chamber depth results were similar in the two cohorts, the prism-based technique demonstrated the  
353 least repeatability and the theoretical technique demonstrated the best repeatability amongst the  
354 three protocols tested. These indicate that results obtained in this study are not limited to the specific  
355 protocol being followed but it reflects a more general trend of one calibration protocol being of lesser  
356 utility than others in obtaining accurate and repeatable estimates of gaze position using 1<sup>st</sup>Purkinje  
357 image-based eye trackers.

358

359 In conclusion, the study demonstrates the existence of inter-and intra-subject variance of the  
360 Hirschberg ratio in all three methods employed to convert the millimetre separation between the 1<sup>st</sup>  
361 Purkinje image and pupil center into angular units. Consequently, using the population-average  
362 Hirschberg ratio may lead to inaccurate estimates of gaze position as shown in the present study. The  
363 prism-based and theoretical techniques both demonstrated relative inaccuracies to the eccentric  
364 viewing technique. However, the prism-based technique showed the poorest repeatability. In  
365 comparison, the theoretical and eccentric viewing techniques demonstrated better repeatability of  
366 Hirschberg ratio.

367

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374

375 References

376 1. Bedell HE, Stevenson SB. Eye movement testing in clinical examination. *Vis Res* 2013;90:32-7.

377 2. Young LR, Sheena D. Survey of eye-movement recording methods. *Behav Res Methods*

378 1975;7(6):397-429.

379 3. Schaeffel F. Kappa and hirschberg ratio measured with an automated video gaze tracker. *Optom*

380 *Vis Sci* 2002;79(5):329-34.

381 4. Raney GE, Campbell SJ, Bovee JC. Using eye movements to evaluate the cognitive processes

382 involved in text comprehension. *J Vis Exp* 2014(83):e50780.

383 5. Eckstein MK, Guerra-Carrillo B, Miller Singley AT, Bunge SA. Beyond eye gaze: What else can

384 eyetracking reveal about cognition and cognitive development? *Dev Cogn Neurosci* 2017;25:69-91.

385 6. Poletti B, Carelli L, Solca F, Lafronza A, Pedroli E, Faini A, Zago S, Ticozzi N, Ciammola A, Morelli C,

386 Meriggi P, Cipresso P, Lule D, Ludolph AC, Riva G, Silani V. An eye-tracking controlled

387 neuropsychological battery for cognitive assessment in neurological diseases. *Neurol Sci*

388 2017;38(4):595-603.

389 7. Brodie S. Photographic calibration of the hirschberg test. *Invest Ophthalmol Vis Sci*

390 1987;28(4):736-42.

391 8. Barry J, Backes A. Limbus versus pupil center for ocular alignment measurement with corneal

392 reflexes. *Invest Ophthalmol Vis Sci* 1997;38(12):2597-607.

- 393 9. Riddell PM, Hainline L, Abramov I. Calibration of the hirschberg test in human infants. Invest  
394 Ophthalmol Vis Sci 1994;35(2):538-43.
- 395 10. Carter AJ, Roth N. Axial length and the hirschberg test. Am J Optom Physiol Opt June  
396 1978;55:361-64.
- 397 11. Model D, Eizenman M, Sturm V. Fixation-free assessment of the hirschberg ratio. Invest  
398 Ophthalmol Vis Sci 2010;51(8):4035-039.
- 399 12. Jagini KK, Vaidyanath H, Bharadwaj SR. Utility of theoretical hirschberg ratio for gaze position  
400 calibration. Optom Vis Sci 2014;91(7):778-85.
- 401 13. Brodie S. Corneal topography and the hirschberg test. Appl Opt 1992;31(19):3627-631.
- 402 14. Bharadwaj SR, Candy TR. Cues for the control of ocular accommodation and vergence during  
403 postnatal human development. J Vis 2008;8(16):14-6.
- 404 15. Eskridge J, Wick B, Perrigin D. The hirschberg test - a double-masked clinical-evaluation. Am J  
405 Optom Physiol Opt 1988;65(9):745-50.
- 406 16. Bharadwaj SR, Candy TR. Accommodative and vergence responses to conflicting blur and  
407 disparity stimuli during development. J Vis 2009;9(11):1-18.
- 408 17. Eskridge J, Perrigin D, Leach N. The hirschberg test - correlation with corneal radius and axial  
409 length. Optom Vis Sci 1990;67(4):243-47.
- 410 18. Roorda A, Campbell MCW, Bobier WR. Slope-based eccentric photorefraction: Theoretical  
411 analysis of different light source configurations and effects of ocular aberrations. J Opt Soc Am A Opt  
412 Image Sci Vis 1997;14(10):2547-556.

- 413 19. Horwood AM, Riddell PM. The use of cues to convergence and accommodation in naive,  
414 uninstructed participants. *Vision Res* 2008;48(15):1613-24.
- 415 20. Koo TK, Li MY. A guideline of selecting and reporting intraclass correlation coefficients for  
416 reliability research (vol 15, pg 155, 2016). *Journal of Chiropractic Medicine* 2017;16(4):346-.
- 417 21. Hasebe S, Ohtsuki H, Tadokoro Y, Okano M, Furuse T. The reliability of a video-enhanced  
418 hirschberg test under clinical conditions. *Invest Ophthalmol Vis Sci* 1995;36(13):2678-685.
- 419 22. Lackner B, Schmidinger G, Skorpik C. Validity and repeatability of anterior chamber depth  
420 measurements with pentacam and orbscan. *Optom Vis Sci* 2005;82(9):858-61.
- 421 23. Crawford AZ, Patel DV, McGhee CNJ. Comparison and repeatability of keratometric and corneal  
422 power measurements obtained by orbscan II, pentacam, and galilei corneal tomography systems.  
423 *Am J Ophthalmol* 2013;156(1):53-60.
- 424 24. Quick M, Boothe R. A photographic technique for measuring horizontal and vertical eye  
425 alignment throughout the field of gaze. *Invest Ophthalmol Vis Sci* 1992;33(1):234-46.
- 426 25. Thaler L, Schuetz AC, Goodale MA, Gegenfurtner KR. What is the best fixation target? the effect  
427 of target shape on stability of fixational eye movements. *Vision Res* 2013;76:31-42.
- 428 26. Thompson JT, Guyton DL. Ophthalmic prisms. *Ophthalmology* 1983;90(3):204-10.
- 429 27. Toole AJ, Fogt N. The forced vergence cover test and phoria adaptation. *Ophthalmic Physiol Opt*  
430 2007;27(5):461-72.
- 431 28. Ukwade M, Bedell H. Stability of oculomotor fixation as a function of target contrast and blur.  
432 *Optom Vis Sci* 1993;70(2):123-26.

- 433 29. Steinman R, Pizlo Z, Forofonova T, Epelboim J. One fixates accurately in order to see clearly not  
434 because one sees clearly. *Spat Vis* 2003;16(3-4):225-41.
- 435 30. Lam A, Chan R, Pang P. The repeatability and accuracy of axial length and anterior chamber  
436 depth measurements from the IOLMaster((TM)). *Ophthalmic Physiol Opt* 2001;21(6):477-83.
- 437 31. Santodomingo-Rubido J, Mallen E, Gilmartin B, Wolffsohn J. A new non-contact optical device for  
438 ocular biometry. *Br J Ophthalmol* 2002;86(4):458-62.
- 439 32. Wang Q, Savini G, Hoffer KJ, Xu Z, Feng Y, Wen D, Hua Y, Yang F, Pan C, Huang J. A  
440 comprehensive assessment of the precision and agreement of anterior corneal power  
441 measurements obtained using 8 different devices. *Plos One* 2012;7(9):e45607.

442

443

444 **Figure legends**

445 **Figure 1:** Raw data of eye position recorded by the PowerRef 3™ plotted as a function of time in the  
446 in eccentric viewing calibration (panel A) and prism-based calibration techniques (panel B) for one  
447 representative emmetropic subject. Positive and negative values in the y-axis indicate leftward and  
448 rightward gaze rotations, respectively, in the eccentric viewing calibration technique. Positive and  
449 negative values in the y-axis indicate the effect of base-out and base-in prisms, respectively, in the  
450 prism-based calibration technique. The right eye was occluded in the eccentric viewing calibration  
451 technique and therefore the instrument did not record any data in this eye (panel A). The right eye  
452 fixated on a distant target while prisms were placed before the left eye that was occluded using an  
453 infrared transmitting filter in the prism-based calibration technique (panel B). Mean (95% CI) of the  
454 eye position data recorded by the PowerRef 3™ plotted as a function of eccentric stimulus position  
455 (panel C) and as a function of prism power (panel D) for the same representative subject. The solid  
456 line through the data represents the best-fit linear regression equation while the dashed line indicates  
457 the unity line.

458

459 **Figure 2:** Box and Whisker plots of the baseline Hirschberg ratios obtained using the eccentric viewing,  
460 prism-based, and theoretical techniques (panel A) and the anterior chamber biometric properties of  
461 the eye (panel B) for calculating the Hirschberg ratio using the theoretical technique in the UU cohort.  
462 The solid horizontal line within the box indicates median value, lower and upper edges of the box  
463 indicate the 25<sup>th</sup> and 75<sup>th</sup> interquartile range and lower and upper whiskers show the 1<sup>st</sup> and 99<sup>th</sup>  
464 quartiles. The squares represent individual data points.

465

466 **Figure 3:** Bland-Altman type plots show the agreement between the Hirschberg ratios obtained using  
467 the three calibration techniques in the UU cohort. Panel A shows the agreement between the prism-  
468 based and eccentric viewing techniques, panel B shows the agreement between the prism-based and  
469 theoretical techniques and panel C shows the agreement between the eccentric viewing and  
470 theoretical techniques. The solid black lines in all panels indicate the mean absolute difference  
471 between the two measurements while the dashed black lines indicate the 95% limit of agreement.  
472 The mean difference (MD) and the limits of agreement (LOA) obtained for each comparison is noted  
473 in the figure panel.

474

475 **Figure 4:** Bland-Altman type plots of repeatability of three calibration techniques in the UU cohort.  
476 Panel A shows repeatability of the eccentric viewing technique, panel B shows repeatability of the  
477 prism-based technique and panel C shows repeatability of the theoretical technique. The solid black

478 lines in all panels indicate the mean difference between the two measurements while the dashed  
479 black lines indicate the 95% limit of agreement. The mean difference and the limits of agreement  
480 obtained for each comparison is noted in the figure panel.

481

482 **Figure 5:** Box and Whisker plots of the baseline Hirschberg ratios obtained using the eccentric viewing,  
483 prism-based, and theoretical techniques (panel A) and the anterior chamber biometric properties of  
484 the eye (panel B) for calculating the Hirschberg ratio using the theoretical technique in the LVPEI  
485 cohort. The solid horizontal line within the box indicates median value, lower and upper edges of the  
486 box indicate the 25th and 75th interquartile range and lower and upper whiskers show the 1st and  
487 99th quartiles. The squares represent individual data points.

488

489 **Figure 6:** Bland-Altman type plots show the agreement between the Hirschberg ratios obtained using  
490 the three calibration techniques (panels A – C) and the repeatability of the prism-based technique  
491 (panel D) in the LVPEI cohort. The solid black lines in all panels indicate the mean absolute difference  
492 between the two measurements while the dashed black lines indicate the 95% limit of agreement.  
493 The mean difference and the limits of agreement obtained for each comparison is noted in the figure  
494 panel.

495

496 **Table 1:** Characteristics, advantages, and disadvantages of the three gaze position calibration techniques.

497 PI – 1<sup>st</sup> Purkinje image, PC – Centre of entrance pupil, AC- Anterior Chamber and HR – Hirschberg Ratio.

Technique	Characteristics	Advantages	Disadvantages
<b>Eccentric-Viewing</b>	<ul style="list-style-type: none"> <li>• Subject fixates on targets placed at known angular eccentricities.</li> <li>• Separation between PI and PC for each target eccentricity is measured.</li> <li>• Reciprocal of slope of linear regression fit of measured separation between PI and PC against target eccentricity gives HR.</li> <li>• Standard calibration routine in most eye trackers.</li> </ul>	<ul style="list-style-type: none"> <li>• Easy to perform in adults and healthy subjects.</li> <li>• Requires minimal technology.</li> </ul>	<ul style="list-style-type: none"> <li>• Assumes that subject is fixating accurately at the expected target location.</li> <li>• Unsteady head position can affect measurement.</li> <li>• Resistance to monocular occlusion in some subjects can make data collection difficult.</li> <li>• Data acquisition can be difficult in uncooperative subjects like infants and children.</li> </ul>
<b>Prism-based</b>	<ul style="list-style-type: none"> <li>• Involves the use of prisms of known base powers to create a separation between PI and PC while one eye is occluded with IR filter</li> <li>• A reciprocal of the slope of the linear regression fit of the separation between the PI and PC against prism power gives the HR.</li> </ul>	<ul style="list-style-type: none"> <li>• Requires minimal technology (loose prisms in a trial case can be used).</li> <li>• Requires minimal participation from subject.</li> <li>• Can be used in infants and children.</li> </ul>	<ul style="list-style-type: none"> <li>• Can be time consuming (e.g. if reflections are present during measurements).</li> <li>• Resistance to monocular occlusion in some subjects can make data collection difficult.</li> <li>• Chance of binocular fusion if monocular occlusion technique is inappropriate.</li> </ul>
<b>Theoretical</b>	<ul style="list-style-type: none"> <li>• HR is derived from anterior chamber biometry of the eye (i.e. corneal curvature and AC depth).</li> <li>• Corneal curvature and AC depth converted into HR using a formula described by Brodie.<sup>7</sup></li> </ul>	<ul style="list-style-type: none"> <li>• HR can be obtained more quickly than other two techniques.</li> <li>• Less reliant on participant's cooperation.</li> <li>• Less reliant on gaze changes</li> </ul>	<ul style="list-style-type: none"> <li>• Dependency on the availability of technology for biometric measures.</li> <li>• Accuracy of HR estimates depends on accuracy and repeatability of the biometric device.</li> </ul>

498

499 **Table 2:** Subject characteristics, experimental set-up and data collection protocols used at the  
 500 University of Ulster (UU) and at the L V Prasad Eye Institute (LVPEI).

<b>Subject details</b>	<b>UU</b>	<b>LVPEI</b>
Sample size	28	30
Age	18 - 40	18 – 40
<b>Refractive error details</b>		
Overall	†0.44 D (25 <sup>th</sup> -75 <sup>th</sup> IQR: -0.13-0.88D)	0.00 D (25 <sup>th</sup> -75 <sup>th</sup> IQR: -2.25 – 0.00D)
i. Myopia	CL corrected, n=9	Uncorrected, n=10
ii. Emmetropia	n=19	n=20
<b>Experimental set up</b>		
Eccentric viewing		
i. Target used	6Maltese crosses	6 LEDs
ii. Viewing distance	2m	3m
iii. Visual angle subtended	± 12° (in 4° steps)	± 15° (in 5° steps)
iv. Fixating eye	Left eye	Left eye
v. Illumination	Dim	Dim
Prism-based		
i. Prism range used	4 – 16ΔD	4 – 25ΔD
ii. Vertex distance	10 – 14mm	10 – 14 mm
iii. IR filter used	Optcast Filter NT3-953	Optcast Filter NT3-953
iv. Fixating eye	Dominant eye	Left eye
Theoretical		
CC and AC depth	Zeiss IOL Master™	Wavelight® Oculyzer™ II
Instrument used		diagnostic device
<b>Data collection protocol used</b>		
Eccentric-viewing		
i. Intra-subject repeatability	Yes (n=28)	No
Prism-based		
i. Intra-subject repeatability	Yes (n=28)	Yes (n=30)
Theoretical		
Intra-subject repeatability	Yes (n=28)	No

501 † Median refractive error for all participants

502 **Table 3:** Repeat measures of median regression slopes, and Hirschberg ratios (HRs) (full range) for  
 503 three calibration techniques and Intraclass Correlation Coefficient (ICC) test of agreement between  
 504 baseline and repeat measures. Baseline values represent first visit measurements. Intra-subject  
 505 variability in each technique was calculated from the MEAN difference (95% Limit of agreement)  
 506 between the baseline and repeat measurements.

	<b>Regression slope (unitless)</b>	<b>Median (full range) HR (°/mm)</b>	<b>Intra-subject variability</b> Mean difference (95% limits of agreement)	<b>Intraclass correlation Coefficient (ICC) rho (95% CI)</b>
<b>UU</b>				
<b>Eccentric viewing</b>				
Baseline	0.99	11.90 (10.61 – 14.63)	0.05 (-0.30 to 0.40) (t=1.63, P=.12)	0.99 (0.98-0.997) P<.001
Repeat measurement	0.99	11.94 (10.28 – 14.29)		
<b>Prism-based</b>				
Baseline	0.89	13.30 (11.47 – 16.93)	0.09 (-1.91 to 2.08) (t=0.44, P=.66)	0.88 (0.74-0.944) P<.001
Repeat measurement	0.87	13.59 (11.34 – 17.83)		
<b>Theoretical</b>				
Baseline	N/A	11.43(9.84 – 13.44)	0.04 (-0.20 to 0.28) (t= 1.93, P= .07)	0.99 (0.99-0.998) P<.001
Repeat measurement	N/A	11.45(9.82 – 13.18)		
<b>LVPEI</b>				
<b>Eccentric viewing</b>				
Baseline	1.04	11.41 (9.52 –14.94)	-	
Repeat measurement	-	-		
<b>Prism-based</b>				
Baseline	0.97	12.16 (10.54 – 15.45)	0.08 (-1.70 to 1.90) (t=0.49, P=.63)	0.83 (0.64 - 0.92) P<.001
Repeat measurement	0.99	11.92 (10.54 – 14.57)		
<b>Theoretical</b>				
Baseline	N/A	11.72 (10.14 – 13.25)	-	
Repeat measurement	-	-		

507 t represents paired t test of the mean difference between baseline measures and repeat  
 508 measurement, and P represents the statistical significance.

509

510

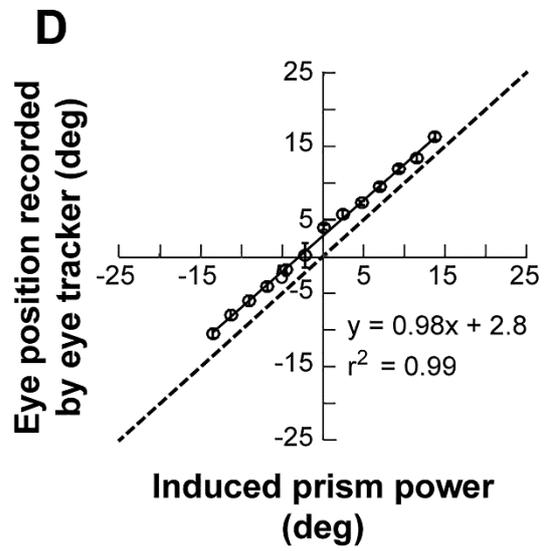
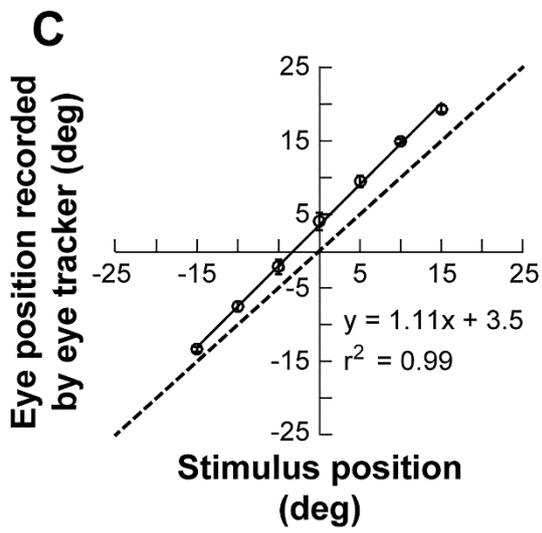
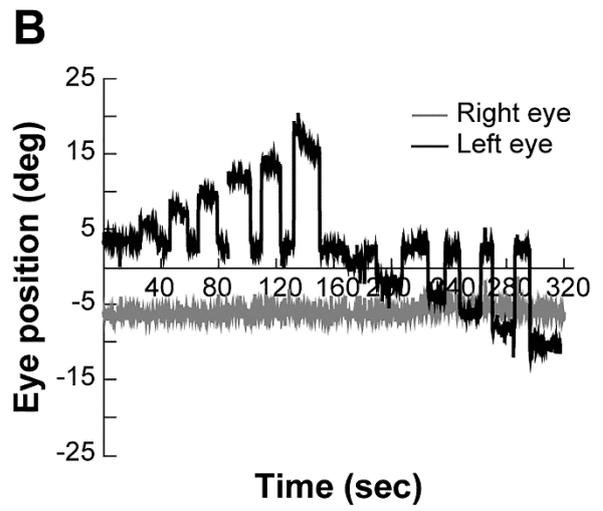
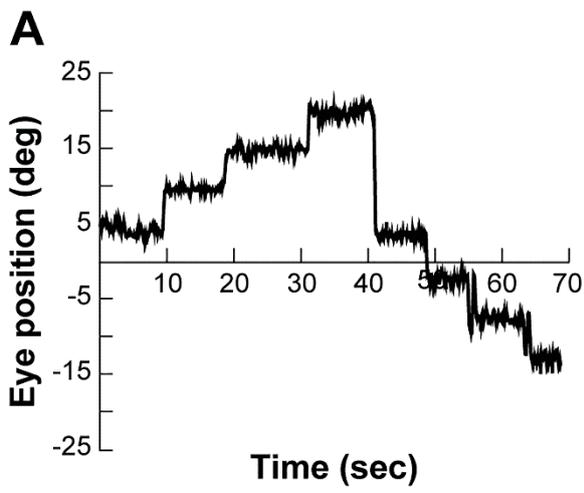
511

512 Table 4. Results of mean signed and mean absolute difference between the three techniques. The  
513 mean signed difference was computed using one-way ANOVA, with post-hoc test employing Scheffe  
514 method. P-values represent probability of mean difference being statistically significantly different  
515 from zero.

	Mean difference (signed) Mean °/mm (95% LOA)	Mean difference(absolute) Mean °/mm (95% LOA)
UU		
Prism-based vs Eccentric viewing technique	-1.63 (-1.17 to 4.43) P<.001	1.87 (-0.27 to 4.01) P<.0001
Prism-based vs Theoretical technique	-2.54 (-0.32 to 5.40) P<.001	2.54 (-0.32 to 5.40) P<.0001
Eccentric viewing vs Theoretical technique	-0.91 (-1.40 to 3.22) P<.024	0.98 (-1.22 to 3.18) P<.001
LVPEI		
Prism-based vs Eccentric viewing technique	-0.77 (-1.58 to 3.1) P<.03	1.11 (-0.63 to 2.85) P<.0001
Prism-based vs Theoretical technique	-0.67 (-0.98 to 2.30) P<.06	0.91 (-0.19 to 2.01) P<.0001
Eccentric viewing vs Theoretical technique	0.10 (-1.73 to 1.53) P=.93	0.57 (-0.61 to 1.75) P<.0001

516 Negative values observed in the 95% LOA for the mean absolute difference column is due to the  
517 mean difference data being skewed, although individual data points were all positive (see Figures  
518 3A-C and 6A-C).

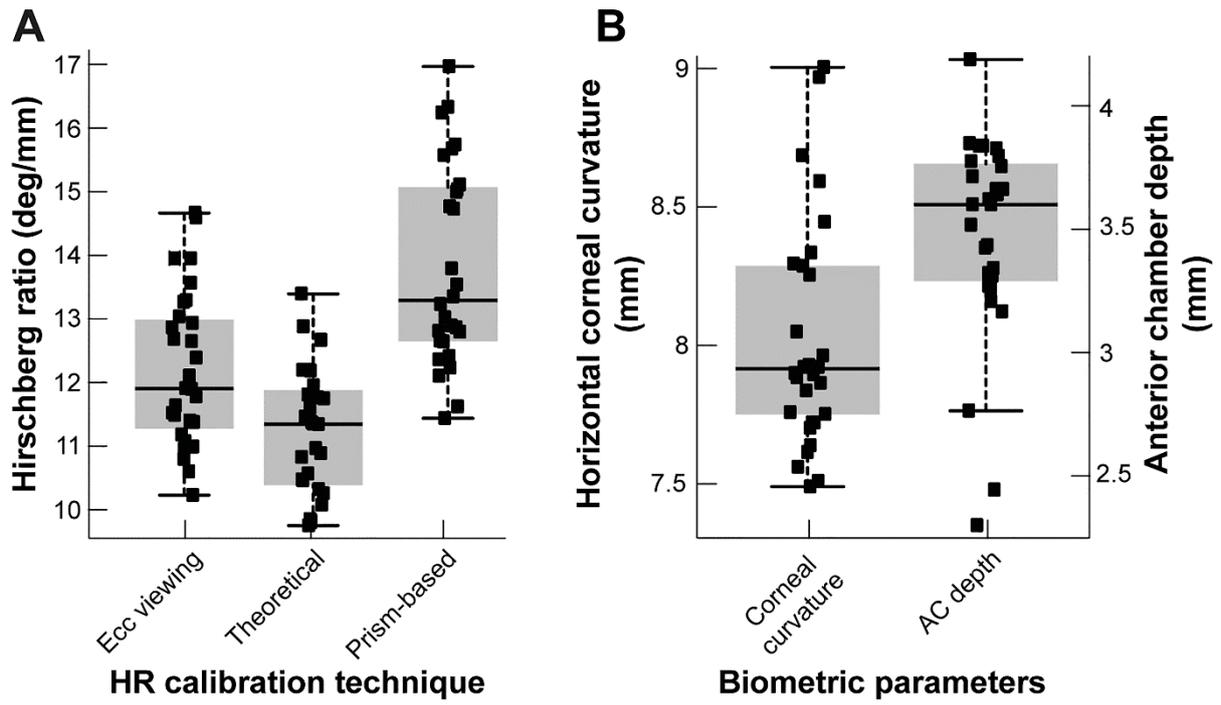
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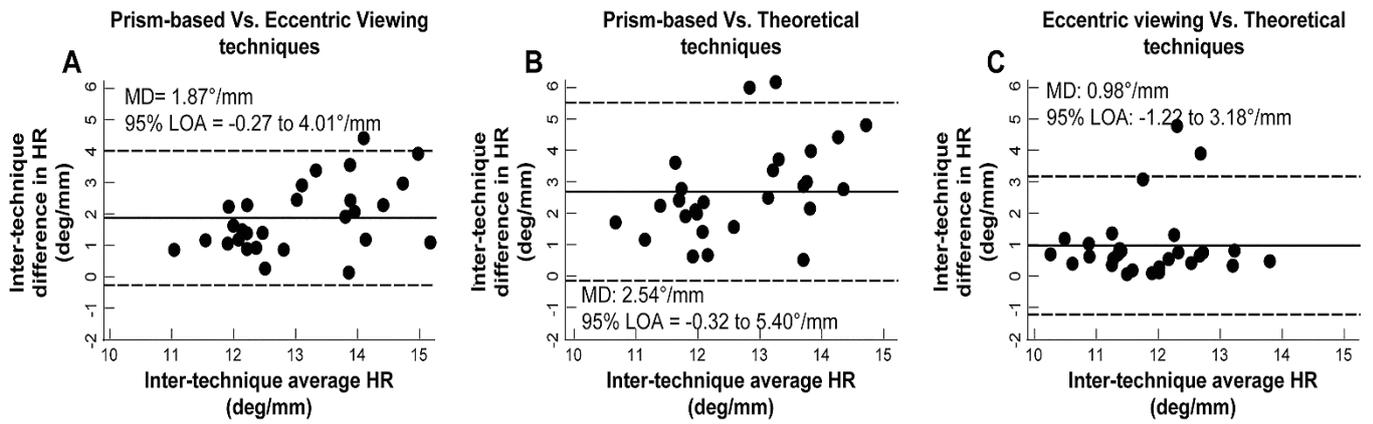
523 Figure 2A-B



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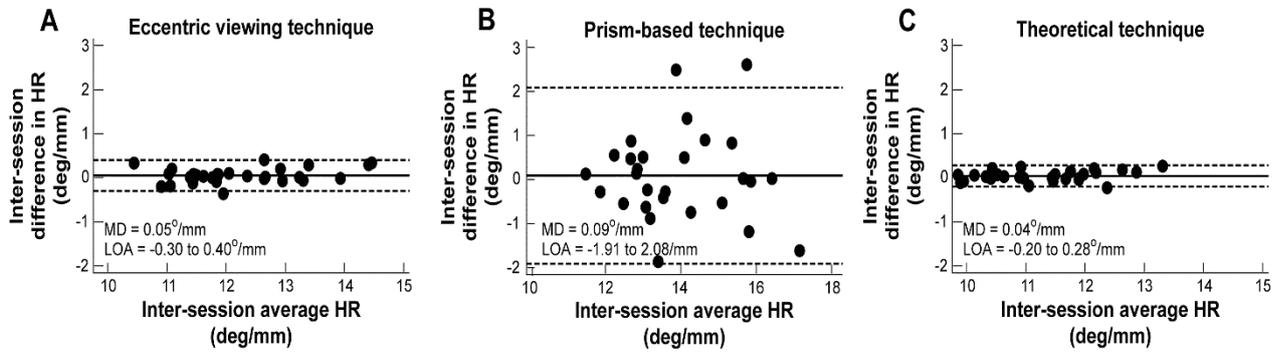
526 Figure 3A-C



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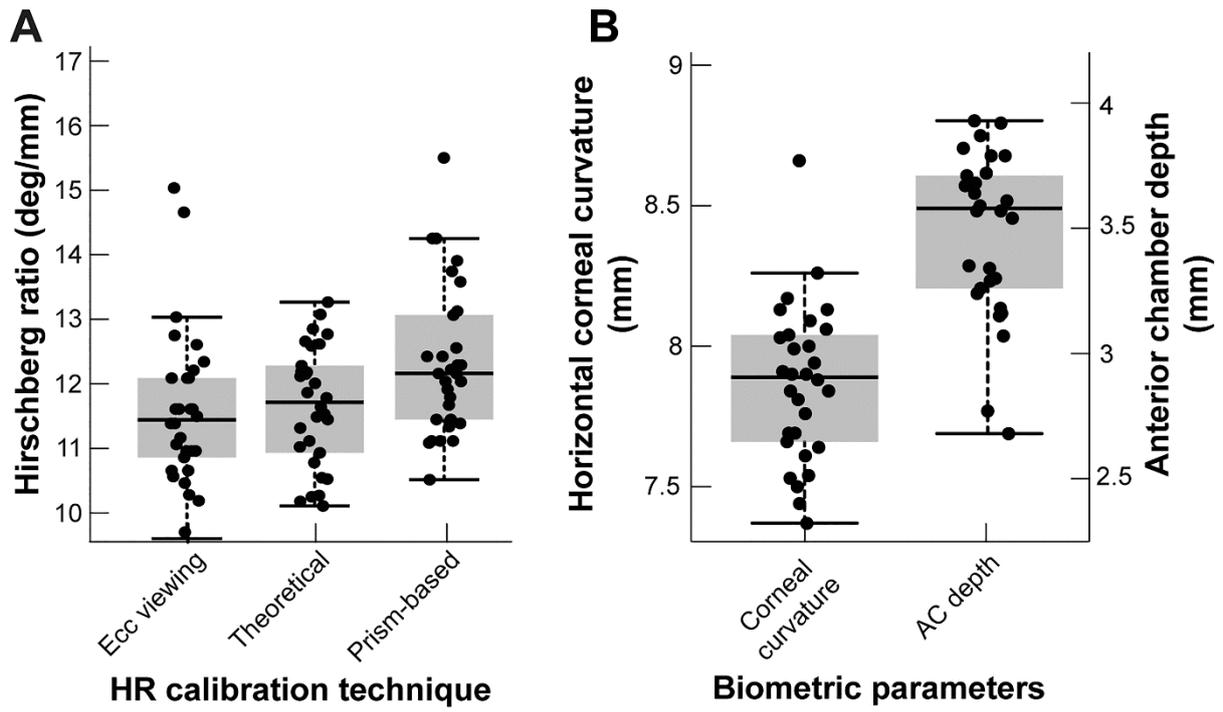
529 Figure 4A-C



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