# Title: Effective *in vivo* topical delivery of siRNA and gene silencing in intact corneal epithelium using a modified cell penetrating peptide

Davide Schiroli1, María J. Gómara2, Eleonora Maurizi1, Sarah D. Atkinson1,3, Laura Mairs1, Kathleen A. Christie1, Diego F. Cobice1, Cian M. McCrudden4, M. Andrew Nesbit1, Isabel Haro2\*, and Tara Moore1\*.

**Affiliations:**

1. Biomedical Sciences Research Institute, University of Ulster, Coleraine, Northern Ireland, BT52 1SA, UK.
2. Unit of Synthesis and Biomedical Applications of Peptides, Department of Biomedical Chemistry, Institute for Advanced Chemistry of Catalonia, Consejo Superior de Investigaciones Científicas (IQAC-CSIC), Barcelona, Spain.
3. Northern Ireland Centre for Stratified Medicine, University of Ulster, Londonderry, BT47 6SB, UK.
4. School of Pharmacy, Queen’s University Belfast, 97 Lisburn Road, Belfast, Northern Ireland BT9 7BL, UK.

\* Correspondence should be addressed to:

T.M., Biomedical Sciences Research Institute, University of Ulster, Coleraine, Northern Ireland, BT52 1SA, United Kingdom. Tel no: +44(0)2870124577. Email:tara.mcmullen@ulster.ac.uk

# ABSTRACT

Autosomal dominantly inherited genetic disorders such as corneal dystrophies are amenable to allele-specific gene silencing with siRNA. siRNA delivered to the cornea by injection, though effective, is not suitable for a frequent long-term treatment regimen, while topical delivery of siRNA to the cornea is hampered by eye surface’s protective mechanisms. Herein we describe an attractive and innovative alternative for topical application using cell penetrating peptide derivatives, capable of complexing siRNA non-covalently and delivering them into the cornea.

Through a rational design approach, we modified derivatives of a cell penetrating peptide, Peptide for Ocular Delivery (POD), already proven to diffuse into the corneal layers. These POD derivatives were able to form siRNA-peptide complexes (polyplexes) of size and -potential similar to those reported able to undergo cellular internalization. Successful cytoplasmic release and gene silencing *in vitro* was obtained when an endosomal disruptor, chloroquine was added. A palmitoylated-POD, displaying the best delivery properties, was covalently functionalized with trifluoromethylquinoline, an analog of chloroquine. This modified POD, named QN-Palm-POD, when complexed with siRNA and topically applied to the eye *in vivo*, resulted in up to 30% knockdown of luciferase reporter gene expression in the corneal epithelium. The methods developed within represent a valid standardized approach, ideal for screening of a range of delivery formulations.

**Keywords:** siRNA, cornea, peptide, CPP, delivery

**Chemical compounds studied in this article**: D-Luciferin potassium salt (Pubmed CID: 23703111); Propylene glycol (Pubmed CID: 1030); Chloroquine (Pubmed CID: 2719); Amphotericin B (Pubmed CID: 5386092).

1. **Introduction**

The eye, and in particular the ocular surface, is one of the most accessible sites for local drug treatment, allowing direct application without the need for systemic administration. This, taken together with the fact that the area to be treated is small and the success of any treatment is easily monitored, makes topical drug delivery an attractive option for ophthalmology. In addition, an immune-privileged status has been proposed which minimizes risk of unwanted side-effects [1](#_ENREF_1),[2](#_ENREF_2).

However, despite its unique attributes, drug delivery through and to the cornea, which represents one of the main components of the ocular surface, has proven to be challenging [3](#_ENREF_3),[4](#_ENREF_4). The main obstacles to achieving a therapeutic dose, by the diffusion of a drug through the eye surface, are the protective mechanisms and underlying ocular anatomy [1](#_ENREF_1),[5](#_ENREF_5). The cornea is a tear film-covered, 500 m deep tissue composed of three layers, from anterior to posterior, the epithelium, stroma and endothelium separated by Bowman’s layer and Descemet’s membrane respectively. A drug may be eliminated from the ocular surface by various mechanisms including lacrimation and tear turnover, drug metabolism and preferential conjunctival absorption [4](#_ENREF_4),[6](#_ENREF_6). The corneal epithelium is a non-keratinized, stratified squamous epithelium, approximately 5–6 cells layers thick, joined together by tight junctions. This, together with the tear film, make the cornea a difficult barrier to overcome and, when the desired target is other parts of the eye, such as the retina, bypass of the cornea by direct injection of the drug (e.g. intravitreal injection) is often the preferred pathway to delivery in the clinic [6](#_ENREF_6),[7](#_ENREF_7).

While methods such as intrastromal injection [1](#_ENREF_1) and iontophoresis [8](#_ENREF_8),[9](#_ENREF_9) have been shown to be successful for delivery to the cornea, the development of a user friendly, non-invasive method such as self-administrated eye drops has proven challenging [10-12](#_ENREF_10). Drugs and delivery agents need to be able to overcome the tear barrier and remain associated with the corneal epithelium for the time necessary to allow cellular internalization. Subsequently once internalized into the target cell the drug cargo must be released to function within the cell with optimal bioavailability.

Among the different drugs for which delivery to the front of the eye is sought, large hydrophilic oligonucleotides represent a unique and effective approach for selective gene therapy treatment of a wide spectrum of corneal diseases [13-15](#_ENREF_13). In particular siRNA-induced gene silencing has been shown to hold great potential for the treatment of different ocular pathologies, reaching phase II and III clinical trials for glaucoma and dry eye [2](#_ENREF_2),[16](#_ENREF_16) and, more recently for corneal pathologies [1](#_ENREF_1),[11](#_ENREF_11) such as corneal dystrophies (CD). CD represent a spectrum of eye diseases associated with one or more different layers of the cornea, affecting its shape, transparency and, in some cases, leading to a partial or complete loss of vision [17](#_ENREF_17). Corneal transplantation is the only intervention that can be used currently in the case of a damaged cornea. CD are frequently caused by missense mutations or small in-frame insertions/deletions [18](#_ENREF_18) and therefore stable gene editing or transient gene silencing are promising tools for a gene therapy approach.

To investigate this further, our group previously developed promising siRNA molecules for a personalized therapeutic approach for CD [19-23](#_ENREF_19). siRNAs that can be used for a transient, reversible, and dosage variable treatment [24](#_ENREF_24),[25](#_ENREF_25), were developed that were highly specific with single nucleotide discrimination at the mutation site [26](#_ENREF_26),[27](#_ENREF_27).

Due to the short half-life of siRNA molecules, a daily, reversible and dosage variable treatment regimen by non-invasive topical delivery is necessary. However, effective delivery remains a challenge and presently no published research reports significant siRNA delivery to an intact corneal epithelium [11](#_ENREF_11),[28](#_ENREF_28).

In addition to overcoming pre-corneal tear film turnover and the other protective mechanisms described, it is necessary to promote cellular uptake of siRNA through the cellular membranes of the epithelial cells and increase corneal bioavailability. Shielding the negatively charged siRNA with positively charged delivery molecules represents a promising option [29](#_ENREF_29). A positively charged formulation can, in the first instance, interact with the negatively charged ocular components, such as the epithelial cell membranes and the external mucus, in order to increase the persistence of the drug on the eye surface [30](#_ENREF_30), and then mediate cellular uptake.

Cationic polymers have been extensively used for drug delivery, in particular of nucleic acids. Examples of these polymers include Polyethylenimine (PEI), Polyamidoamine dendrimers (pAMAM) and Chitosan, which are routinely used for cell transfection *in vitro* and *in vivo* [31](#_ENREF_31). Different cationic polymers may be used to deliver oligonucleotides to the eye surface [32](#_ENREF_32) and among these cationic cell-penetrating peptides (CPPs) are very versatile and promising [33](#_ENREF_33). Their positive charges can be exploited both to generate an ionic interaction with the negatively charged siRNA and to drive ocular penetration and, when compared with other nanoparticles, CPPs have the advantage of forming nanoparticles by simply mixing the peptide with siRNA in aqueous solution. CPPs have been used extensively to deliver various macromolecules [34](#_ENREF_34), including siRNA [35](#_ENREF_35),[36](#_ENREF_36), to cells, both *in vitro* and *in vivo*. They can be easily modified by the addition of chemical blocks to address different delivery hurdles, for example lipid moieties (such as palmitoyl- and cholesteryl-) may be added in order to increase the hydrophobicity of CPPs and thus favor the destabilization of the endosomal membrane. CPPs can also be used together with other molecules involved in delivery, offering a wide range of potential combinations. Moreover, in contrast to other cationic polymers, CPPs are well defined chemical entities, allowing a better control of the CPPs:siRNA molar ratio.

CPPs, such as POD [37](#_ENREF_37),[38](#_ENREF_38) and PEP-1 [39](#_ENREF_39), have demonstrated ability to penetrate the corneal tissues when applied topically to the eye. Herein, we present the development of a modified POD for corneal delivery of siRNA that overcomes poor endosomal escape (when siRNA remains trapped in endosomes and is trafficked into lysosomes where it is degraded) [34](#_ENREF_34),[35](#_ENREF_35),[40](#_ENREF_40). In this study, chloroquine (Chlq) [41](#_ENREF_41) was firstly applied together with the polyplexes (i.e. nucleotides-peptide complexes [42](#_ENREF_42)) to elicit siRNA release from the endosomes, in order to confirm the endosomal entrapment and to determine if a lysogenic compound was able to enhance siRNA release *in vitro* and *in vivo*. Subsequently, the combination that showed the best delivery properties when tested *in vitro* and *in vivo* was selected and covalently modified with a chloroquine analog. A corneal epithelium cell line was used as an *in vitro* model while *in vivo* experiments were performed on a novel murine model expressing, under the regulation of the corneal specific *Krt12* promoter the luciferase gene and Meesmann epithelial CD mutations.

This covalently modified peptide, once topically applied on the eye surface, proved capable of delivering bioavailable siRNA into corneal epithelial cells, allowed effective release of the siRNA from the endosomes and achieved significant knockdown of gene expression.

# Results

# *Evaluation of in vitro siRNA delivery using modified versions of Peptide for Ocular Delivery (POD)*

# To improve the delivery and bioavailability of siRNA by the POD peptide, novel chemical modifications were introduced (Table 2). To minimize the number of possible candidates to be tested *in vivo* with the mouse corneal reporter model, the different modified versions of POD were first tested to determine their delivery activity *in vitro* in a corneal epithelial cell model [43](#_ENREF_43).

Initially, POD was modified with either a palmitoyl group, a cholesteryl group, or PLGA-PEG and tested for its ability to deliver siRNA in corneal epithelial cells. POD was functionalized with a palmitoyl- or a cholesteryl- group as these modifications, increasing the ability of a peptide to fuse with the plasma membrane, were previously shown to enhance the performance of other siRNA delivering peptides [44](#_ENREF_44),[45](#_ENREF_45). PLGA-PEG-POD was selected for this study as PEG-POD was reported to efficiently deliver nucleotides *in vivo*, while the addition of PLGA was shown to enhance the capability of PEG-POD to penetrate corneal tissues [37](#_ENREF_37),[46](#_ENREF_46).

 *3.1.1 Evaluation of POD-siRNA complexes*

A molar ratio of 35:1 POD:siRNA was used to determine the PODs-siRNA complex formation in a gel retardation assay. This molar ratio was chosen as molar ratios between 30:1 and 50:1 have been demonstrated previously to result in the maximum incorporation of siRNA into complexes for other CPP [47](#_ENREF_47). Moreover, a molar ratio of 25:1 was shown to achieve efficient knockdown of GFP expression in transiently transfected cells [38](#_ENREF_38); while Haro *et al.* determined the cell viability in cells treated with the PLGA-PEG-POD to be higher than 60% at a concentration of 2.5 mg/ml (herein we used 1.4 mg/ml PLGA-PEG-POD) [37](#_ENREF_37),[38](#_ENREF_38). At 35:1 molar ratio, Chol-POD, Palm-POD, PLGA-PEG-POD and POD all showed complete complexation of siRNA (Figure 1A). Uncomplexed siRNA (siRNA only) migrates into the agarose gel, while siRNA complexed with PODs does not escape from the wells; this POD:siRNA ratio was used for all further experiments.

 *3.1.2 PODs* *-potential and size*

CPP-siRNA complexes that have the highest rate of endocytic uptake and tissue diffusion are generally smaller than 200 nm [47](#_ENREF_47) and have a positive -potential (generally lower than +40 mV) in aqueous solution [47-49](#_ENREF_47). The size and -potential of each POD-siRNA complex was therefore determined. The analysis showed that the particles from each formulation in PBS, had mean diameters and mean charges (Table 1) that fall within the described parameters and are thus suitable for cell delivery. The analysis was also performed in water to assess if a buffered pH may have an effect on the properties of the complexes (data not shown). However only a minimal reduction of the charge and dimension was observed when prepared in PBS, which was used from this point to prepare the other formulations described in study.

 *3.1.3 Evaluation of siRNA cellular delivery*

A human epithelial corneal epithelial cell line (HCE-S) [50](#_ENREF_50) was used for initial *in vitro* screening in order to evaluate cellular transfection and toxicity properties of the POD-siRNA complexes and to reduce the number of animals needed for the subsequent *in vivo* analysis. Although corneal epithelial cell lines have molecular features that differ from the original epithelium [51](#_ENREF_51) and might respond differently to the treatment if grown in different culture conditions [52](#_ENREF_52) they represent a valid cellular model of the cornea to initially investigate cellular transfection and toxicity [53](#_ENREF_53). Delivery of a green fluorescently-labeled non-targeting siRNA (siGLO) into HCE-S cells by each of the different PODs was tested. The majority of HCE-S cells, transfected with all three different POD-siRNA formulations showed punctuate cytoplasmic fluorescence (Figure 1B) with a perinuclear concentration (nuclei stained blue, DAPI), in agreement with previous observations in corneal epithelial cells of a rabbit cornea treated with fluorescently labelled POD [37](#_ENREF_37). No intracellular fluorescence was detectable in cells treated with non-complexed siGLO (Figure 1B). The perinuclear distribution pattern of the POD-delivered siGLO is characterized by fluorescent dots, larger than those observed using the commercially available cationic lipid transfection agent RNAiMAX (Figure 1B). The perinuclear distribution of fluorescence suggests that the nanoparticles are internalized along an endocytic pathway [47](#_ENREF_47),[54](#_ENREF_54),[55](#_ENREF_55).

 *3.1.4 Evaluation of POD cellular toxicity*

siRNAs used herein were previously reported not to elicit any toxicity or immunological response in HCE-S cells[43](#_ENREF_43). The cellular toxicity of PODs:siRNA complexes were assessed by measuring cell viability using an MTT assay in HCE-S cells treated for 24 hours with PODs at different concentrations (Figure 1C). Under these conditions, cells treated with Chol- and Palm-POD showed, when compared to the untreated control, an ~87% and 75% cell viability with 17.5 M and 35 M POD that fell to ~55% at 70 M. PLGA-PEG-POD was instead showing ~100% viability. Similar results were obtained for the POD-siRNA comparison, showing that the presence of Chol-, Palm- and PLGA-PEG groups did not elicit cellular toxicity.

 *3.1.5 Evaluation of gene knockdown*

The 35:1 PODs:siRNA ratio, determined by a gel retardation assay to be sufficient for complexing all the siRNA, was then used to assess knockdown of luciferase reporter gene expression in HCE-S cells using a dual-luciferase assay, as previously described [26](#_ENREF_26),[56](#_ENREF_56). No significant knockdown was observed when cells were transfected with luciferase targeting siRNA (siLuc) complexed with any of the four different PODs(black bars) compared to PODs complexed with non-targeting siRNA (NSC4) (grey bars) (Figure 1D), while knockdown was achieved in the positive control, using RNAiMAX (p<0.001). The results obtained are consistent with those previously observed in studies with other CPPs where, even in case of strong cell association, no significant gene expression knockdown was measured [47](#_ENREF_47).

*3.2 Evaluation of endosomal release*

Since all the PODs tested were able to deliver siRNA *in vitro* but failed to knockdown luciferase expression, we hypothesized that the siRNA-peptide complexes were entrapped in endosomes, a well-known cellular barrier that prevents the cytosolic release of siRNAs [57-59](#_ENREF_57). To test this hypothesis, assessment of delivery and knockdown was repeated, treating the cells with the POD-siRNA formulations together with Chloroquine (Chlq) [41](#_ENREF_41), reported to increase endosomal escape. This should result in a release of siRNA to the cytoplasm where it can target mRNA and be observed as reduction in luciferase reporter expression.

In combination with Chlq, PODs:siRNA-complexes were observed in a more diffuse cytoplasmic pattern (Figure 2A) when compared to the same complexes without Chlq (Figure 1B), and achieved a significant knockdown of luciferase expression. (Figure 2B). Based on these *in vitro* analyses Chol- and Palm-POD were selected for the subsequent *in vivo* experiments. In further experiments, these two PODs were tested to identify which demonstrated the best *in vivo* delivery and might be thus covalently modified with an endosomal disruptor. Direct derivatization of a POD is sought to maximize endosomal release whilst minimizing corneal toxicity. PLGA-PEG-POD was excluded from this *in vivo* comparison as its chemical and structural features made it unsuitable for any further chemical derivatization.

*3.3 Corneal delivery and knockdown of luciferase expression by intrastromal injection of Accell-siRNA*

Previous *in vivo* studies have demonstrated that direct intradermal injection of siRNA can: (i) specifically silence co-injected target alleles in murine epidermis [27](#_ENREF_27),[60](#_ENREF_60),[61](#_ENREF_61); (ii) silence expression of epidermal reporter transgene [62](#_ENREF_62); and (iii) show efficacy in a Phase 1b clinical trial [63](#_ENREF_63). “Pressure-fection” intrastromal injection of plasmid into the corneal stroma has been shown to result in GFP expression in all layers of the cornea [64](#_ENREF_64),[65](#_ENREF_65). To determine whether the siLuc siRNA was able to knockdown luciferase expression in the cornea of the *Krt12*+/*luc2* mice, we first sought to demonstrate that intrastromal injection can deliver siRNA to all layers of the murine cornea. Live animal imaging was performed following intrastromal injection of Cy3-labelled Accell siRNA, a nuclease-resistant siRNA with ‘self-delivery’ properties [27](#_ENREF_27). Strong fluorescent signals were observed in the mouse eye for up to 72 hours following injection, however, the signal was most intense at 6 hours post-injection (Figure 3A). Fluorescence microscopy showed that Cy3-labelled Accell siRNA localised to the corneal epithelium and stroma after the initial injection, with pronounced distribution within the corneal epithelium visible 6 hours after injection (Figure 3B). The fluorescence in the stroma declined within 12 hours. These findings confirmed that intrastromal injection results in siRNA delivery to the corneal epithelium and suggest that the retention times should be sufficient to study siRNA gene silencing in living *Krt12+/luc2* mice.

In order to assess the ability of the described siRNAs to knockdown the expression of the luciferase gene *in vivo*, intrastromal injections of Accell modified siRNA in mice expressing luciferase in the cornea were performed.

Before *in vivo* treatment experiments began, corneal luciferase activity in *Krt12*+/*luc2* mice was quantified every 24 hours for 3 days to confirm a consistent right-to-left ratio. Accell control (Accell-NSC4) or luc2 siRNAs (Accell-siLuc) were delivered by intrastromal injection (n= 3 mice/group) and corneal epithelial luciferase expression evaluated daily by live animal imaging over 7 days (Figure 3C). Accell-siLuc inhibited luciferase expression *in vivo*, with >50% repression achieved 72 hours post-injection. Maximal inhibition (64%) was observed at day 5 and silencing persisted at day 6 (Figure 3D); data were statistically significant (p<0.05) for both time points. Importantly, intrasomal injection of non-targeting Accell-NSC4 had no significant effect (Figure 3D).

In parallel experiments, no significant knockdown of expression was observed when luciferase expression was measured following topical application of Accell siRNA (data not shown). Therefore, to investigate whether siRNA-POD polyplexes can mediate knockdown of corneal gene expression following topical application, we chose to use the siLuc siRNA that we had proven to knockdown luciferase expression *in vivo* by intrastromal injection. However, we combined PODs with native and not Accell-modified siRNA as it is not known whether this modification interferes in the peptide-siRNA interaction and CPP-mediated delivery.

*3.4 In vivo evaluation of topical delivery of POD-siRNA complexes to the cornea using a fluorescent siRNA*

Following the demonstration that successful delivery and gene knockdown *in vitro* was facilitated by the addition Chlq*,* the two modified versions of the POD (Palm-POD and Chol-POD) were assessed for *in vivo* delivery of siRNA. PODs were first complexed with red fluorescent siGLO at the same molar ratios used for *in vitro* delivery, applied topically to the eye surface of wild-type mice and fluorescence was monitored for up to 24 hours. All the eyes treated with siGLO in combination with a POD showed fluorescence up to 24 hours, while the siGLO only-treated eyes did not show any visible fluorescence (Figure 4A). At 3 and 6 hours after application, fluorescence signals from siGLO-Palm-POD and of siGLO-Chol-POD were significantly higher than the siGLO only control. siGLO-Palm-POD fluorescence was between three and four times more intense than the one measured for Chol-POD (Figure 4B).

24 hours after the application of POD-siRNA, the eyes were collected and distribution of the siRNA throughout the cornea observed. Red fluorescence was detected in all the treated sections throughout the corneal layers, particularly the corneal epithelium, while no fluorescence above background was observed in the siGLO only control (Figure 4C).

Since PODs alone are not sufficient to deliver siRNA into the cytoplasm, with the siRNA-POD complexes probably retained into the endosomes, and Chlq has been proven to elicit endosomal escape *in vitro*, but is known to result in *in vivo* toxicity [66](#_ENREF_66), we decided to covalently modify POD with an analog of Chlq that shows low toxicity. We also chose to use Palm-POD rather than Chol-POD as it showed a better delivery of siGLO *in vivo* (Figure 4B).

# *3.5 Evaluation of in vitro and in vivo siRNA delivery using a palmitoylated version of Peptide for Ocular Delivery (POD) functionalized with chloroquine (QN)*

# An analog of Chlq, trifluoromethylquinoline (QN), was selected to covalently functionalize Palm-POD as a peptide previously developed for siRNA delivery was similarly derivatized, and showed successful *in vivo* delivery with low toxicity [67](#_ENREF_67) (Figure 5A).

 *3.5.1 Evaluation of PODs-siRNA complexes*

To assess whether the functionalization of Palm-POD with QN altered the ability of the POD to bind siRNA and to determine the optimum ratio of QN-Palm-POD:siRNA for POD-siRNA complex formation, QN-Palm-POD was titrated at different molar ratios with siRNA. Whilst partial complexation of siRNA was observed at 35:1 and 70:1 (with slightly more siRNA bound to the POD at 70:1 molar ratio), a 140:1 molar ratio achieved complete siRNA complexation (Figure 5B). This result suggests that the presence of the covalently attached QN molecule reduces the ability of the peptide to interact with siRNA by approximately 75% as a 35:1 molar ratio of Palm-POD:siRNA was sufficient to achieve complete complexation (Figure 1A).

 *3.5.2 QN-Palm-POD ζ-potential and size*

Biophysical Analysis of the QN-Palm-POD-siRNA complexes (140:1 ratio) showed that they had a mean diameter (± SD) of 107.1 ± 3.2 nm and a mean charge (± SD) of +14.9 ± 4.2 mV in PBS (Table 2). Thus, the presence of the QN groups does not have an effect on the charge of complexes formed in PBS (14 mV), and while the dimensions of the QN-Palm-POD complexes are reduced compared to Palm-POD, in PBS (142 nm to 107 nm), these values remain in the range suitable for cellular delivery (as described in section 3.1.2 [47-49](#_ENREF_47)).

* + 1. *Evaluation of QN-Palm-POD cellular toxicity*

Cellular toxicity of QN-Palm-POD-siRNA in HCE-S cells treated with POD concentrations of 9, 17.5 and 35 M (140:1 molar ratio) was measured with an MTT assay (Figure 5C). Cell viability was reduced to ~80% in cells treated with 9, 17.5 and 35 M QN-Palm-POD when compared to untreated cells.Thus, to achieve complete complexation of siRNA (140:1 molar ratio) while minimizing cellular toxicity, the concentrations used for the transfection experiments of QN-Palm-POD and siGLO/siLuc were reduced to 17.5 M and 125 nM, respectively.

* + 1. *Evaluation of siRNA cellular delivery*

To investigate the effect of Palm-POD functionalization with QN, 17.5 M QN-Palm-POD complexed with 125 nM siGLO (molar ratio of 140:1) was used to transfect HCE-S cells. Efficient transfection (>90%, counting nuclei surrounded by fluorescent green dots) was achieved (Figure 5D). siGLO is distributed in the cells with a punctuate pattern both around the nuclei and throughout the cytoplasm. When compared with the non-functionalised Palm-POD, the fluorescent dots have a reduced dimension and are less defined, more similar in appearance to that observed in RNAiMAX transfected cells. This suggests an endocytic uptake, but also an improved endosomal release.

* + 1. *Evaluation of knockdown of reporter gene expression*

Knockdown of luciferase reporter gene expression was assessed in HCE-S using QN-Palm-POD:siLuc complexes. 72 hours after transfection, a 50% knockdown of luciferase expression (p<0.05) was observed. Although, addition of 30 M Chlq to the QN-Palm-POD:siLuc complex transfected cells increased knockdown of luciferase gene expression to 62% (p<0.01), this was not significantly higher than with QN-Palm-POD:siLuc complex alone. (Figure 5E).

* + 1. *In vivo evaluation of QN-Palm-POD-siRNA complex delivery to the cornea*

To assess the ability of the QN-functionalised POD to deliver siRNA *in vivo*, fluorescence was measured as described above using a 140:1 molar ratio (700 M QN-Palm-POD and 5 M siGLO), following topical application of siGLO-QN-Palm-POD complexes. Although the fluorescence intensity was lower than that observed for the non-functionalised Palm-POD fluorescence in the cornea treated with QN-Palm-POD-siRNA persisted for up to 24 hours (Figure 6A) and is significantly higher than in corneas treated with the siGLO alone at all the time points (p<0.001 at 3 hours, p< 0.05 at 6 and 24 hours) (Figure 6B). Sections of the treated corneas show uptake of siGLO in all the corneal layers (epithelium, stroma and endothelium) (Figure 6C), while siGLO was not observed in the posterior segment (data not shown).

* + 1. *In vivo evaluation of QN-Palm-POD-siRNA nanoparticle knockdown of luciferase expression*

# The ability of QN-Palm-POD to deliver siRNA to the cornea and achieve knockdown of corneal epithelial gene expression *in vivo* was assessed using siLuc knockdown of luciferase expression in a *Krt12+/luc2* mouse model. In a split body control experiment, mice (n=5) were treated with QN-Palm-POD complexed with siLuc (right eye) and NSC4 (left eye) (140:1 molar ratio with 700 M QN-Palm-POD and 5 M siRNA) in parallel, daily for four days. NSC4 was shown earlier not to decrease luciferase signal when injected in the stroma, suggesting that any observed effect on luciferase gene expression is not due to non-specific or toxic effects.

# Although no significant knockdown of expression was observed during the four days of treatment, a significant knockdown was detected in the three days following the termination of the treatment with *QN-Palm-POD-siRNA* reaching a maximum of 30% (p <0.001) at day 9 (day 3 after withdrawal of treatment) (Figures 6D and E), while luciferase gene expression returned to pretreatment level 4 days after treatment.

 *3.5.8 In vivo evaluation of cellular toxicity*

To assess whether topical application of QN-Palm-POD-siRNA complexes caused toxicity and damage to the cornea, corneal sections of the treated eyes collected after the termination of the experiment were examined but did not show any alteration of the corneal layers, nor signs of inflammation or cellular infiltration(Figure 6F). Mice eyes were examined by an ophthalmic surgeon at various time points during treatment and up to 15 days post-treatment and all eyes presented as quiet eyes. At no time point were any signs of swelling, oedema or inflammation noted.

# Discussion

The results presented here are the first example of successful topical delivery of a mixed siRNA-delivery agent to the cornea. siRNAs have been successfully and extensively used to treat different diseases [68](#_ENREF_68) but their application for the treatment of corneal pathologies has proven to be difficult, despite the external accessibility of this organ [1](#_ENREF_1),[11](#_ENREF_11),[28](#_ENREF_28). To date, administration of oligonucleotides by intrastromal injection is the preferred route [6](#_ENREF_6),[65](#_ENREF_65),[66](#_ENREF_66) although not suitable for a prolonged and repeated treatment regimen [69](#_ENREF_69). Commercially available transfection agents transfection agents, including Lipofectamine 2000, Entranster-in vivo, polyethyleneimine (PEI) and PEO-PPO-PEO polymers are unable to deliver Cy3-siRNA to mouse cornea *in vivo* [11](#_ENREF_11).

For successful polynucleotide delivery a vehicle should fulfil three requirements: 1) delivery to the desired tissue, 2) release of cargo into the cytoplasm 3) low toxicity. Cell penetrating peptides have been proven to satisfy all these requirements, delivering siRNA and peptides to cells [57](#_ENREF_57),[70](#_ENREF_70), with an increasing number of peptides used for this purpose [34](#_ENREF_34),[47](#_ENREF_47),[71-74](#_ENREF_71). Some CPPs have been used *in vivo* to deliver siRNA, targeting tumors, the brain-blood barrier, and other tissues [75](#_ENREF_75),[76](#_ENREF_76) but none topically applied, either to the skin or the ocular surface [34](#_ENREF_34). A CPP with proven ability to overcome the corneal barrier [37](#_ENREF_37),[38](#_ENREF_38), Peptide for Ocular Delivery (POD) with a PEG moiety showed improved functionalizing [77](#_ENREF_77) able to deliver a luciferase expression vector to retinal cells *in vivo* [46](#_ENREF_46),[77](#_ENREF_77),[78](#_ENREF_78) and more efficiently than other CPPs such as HIV-Tat and CK30 [77](#_ENREF_77). Further modification of PEG-POD by the addition of one moiety of PLGA, previously proven to be biomedically compatible and with recognized delivery features [36](#_ENREF_36),[37](#_ENREF_37), resulting in PLGA-PEG-POD, improved the *in vivo* bioavailability of POD [37](#_ENREF_37).

In the present study, we compared PLGA-PEG-POD with the native POD and two other PODs modified with either a palmitoyl- or a cholesteryl- group (Palm-POD and Chol-POD), in an attempt to improve the performance of siRNA delivery [44](#_ENREF_44),[45](#_ENREF_45). Cholesterol-functionalized siRNAs have been extensively used for this purpose, and their therapeutic use has progressed to clinical trial [79](#_ENREF_79); palmitoylation has proved to enhance peptide absorption by the lipid bilayer of the cell membrane [80](#_ENREF_80),[81](#_ENREF_81).

*In vitro*, all the PODs tested were able to achieve cellular delivery of siRNA with a low toxicity, which did not exceed that previously reported for the cationic lipid transfection agent, lipofectamine [82](#_ENREF_82) and CPPs at high concentrations [47](#_ENREF_47). However, bioavailability was not achieved and none of the formulations achieved gene silencing of a luciferase reporter gene in *in vitro* transfected HCE-S cells, consistent with other CPPs, where cellular delivery of siRNA was not matched with gene silencing [47](#_ENREF_47).

We attributed the lack of bioavailability and gene silencing in cells treated with POD-siRNA complexes to endosomal entrapment, assuming whichever internalization pathway is utilized by CPP [73](#_ENREF_73), it is fundamental to develop a method that permits the siRNA to escape from the endosomes [35](#_ENREF_35). Herein, we demonstrated chloroquine, a known endosomal disruptor (coupled to, and derivatized with the POD peptide), to elicit siRNA endosomal release and gene silencing, in agreement with previous reports [41](#_ENREF_41),[54](#_ENREF_54),[83](#_ENREF_83). However, the structural and chemical features of PLGA-PEG-POD, make it unsuitable for further covalent modification with endosomal disruptors and since the latter are essential to improve the release and decrease corneal toxicity, PLGA-PEG-POD was excluded from the *in vivo* study. Both Palm- and Chol-POD achieved a significantly higher knockdown than the POD and they were thus selected for the subsequent *in vivo* analysis.

Topical drug delivery to the eye surface has proven difficult due to several anatomical barriers. The tear film in particular reduces the contact time of an applied drug to the eye surface. Absorption through the conjunctival pathway is responsible for the removal of more than 75% of any administrated drug on the ocular surface [84](#_ENREF_84). Topical delivery of POD to the cornea is promising: a fluorescently tagged POD was visible in mouse corneas 45 minutes after application and persisted, with a decreased intensity, for 24 hours afterwards, penetrating into the different corneal layers [38](#_ENREF_38). Similarly, a fluorescently labelled PLGA-PEG-POD was visible in rabbit corneas 2 hours after topical application [37](#_ENREF_37). siRNA alone cannot penetrate *in vivo* into the murine cornea unless injected under pressure into the stroma. In comparison topical delivery of siRNA combined with Chol- and Palm-POD effectively penetrated into all corneal layers and demonstrated some gene silencing of the target gene. The persistence of the fluorescent siRNA for up to 48 hours after topical application suggests that these PODs have the capacity to interact with the ocular surface, thus increasing the effective time of exposure and the amount of complex that can be internalized, which is in contrast to results previously described for modified, single filament fluorescent siRNA, completely cleared from the cornea in about 3 hours [85](#_ENREF_85).

We demonstrate here that to achieve knockdown of gene expression an endosomal disruptor, like Chlq, is necessary to release the siRNA into the cytoplasm. However, since Chlq has been reported to display strong systemic and corneal toxicity [66](#_ENREF_66) we sought a way to use it *in vivo* that would minimize these harmful side-effects. An analogue of Chlq, trifluoromethylquinoline (QN), linked to the peptide PepFect6, was previously shown to deliver siRNA and miRNA and achieve knockdown, both *in vivo* and *in vitro* [67](#_ENREF_67),[86](#_ENREF_86) without significantly enhancing cytokine levels in serum and cellular toxicity in kidney, lung, liver and spleen [67](#_ENREF_67),[87](#_ENREF_87). We modified Palm-POD by the covalent addition of two moieties of QN. The ability of the Palm-POD to complex siRNA was reduced by QN-functionalisation, probably due to the presence of the bulky QN moiety and, to compensate for this, subsequent *in vitro* experiments were all conducted with a 140:1 molar ratio and 125 nM siRNA. Enhanced endosomal release was confirmed through bioavailability and significant knockdown of luciferase expression 72 hours after transfection, which was not significantly increased when the cells were pre-treated with Chlq.

The functionalized formulation was also able to deliver siRNA *in vivo*, performing as well as unmodified Palm-POD, with the siGLO fluorescent signal persistent in the cornea for up to 24 hours. This is despite the fact that, as a consequence of the reduced complexation capacity of QN-Palm-POD, the amount of siGLO applied was reduced. Furthermore, the luciferase reporter gene expression knockdown observed (up to 30%) in the corneal epithelium was greater than previously achieved despite a reduced amount of siRNA and the effect was prolonged for three days after treatment, and had no observable toxic or inflammatory effect on the cornea *in vivo*. Enhancing gene silencing within the cornea, using non-invasive eye drop delivery, to a therapeutic level remains a challenge and we have not matched the 60% knockdown previously reported in mice skin using Accell-siRNA [62](#_ENREF_62). We can match this level of corneal gene silencing using intrastromal injection of Accell siRNA (64%) as described within, but this is not suitable for repeated and long term siRNA therapeutic application in the ophthalmology clinic. To our knowledge, the modest 30% gene silencing result we achieved is the first report of a decreased protein expression in corneal epithelium after siRNA mediated knockdown persisting up to 72 hours after eye drop treatment. Taketani *et al.* observed knockdown in mouse cornea only at the mRNA level and only for 24 hours after the treatment, while mRNA expression returned to the untreated level by 48 hours [85](#_ENREF_85).

Moreover, in agreement with reports that PepFect6-siRNA does not elicit an inflammatory response *in vivo* [67](#_ENREF_67),[87](#_ENREF_87) and does not alter the lipid bilayer [88](#_ENREF_88), no toxic effect of QN-Palm-POD-siRNA was observed in mouse corneas *in vivo*, suggesting that the reduced amount of this chloroquine analog is not toxic to the corneal epithelium.

In summary, we designed a novel version of a cell penetrating peptide for ocular delivery (POD) capable of complexing the siRNA, delivering it into the corneal layers and releasing functional siRNA into the cytoplasm which ultimately results in targeted gene expression reduction.

Palmitoyl-POD-siRNA complex gave the best knockdown of *in vivo* gene expression and, when chemically modified by covalent attachment of the Chlq analogue, trifluoromethylquinoline (QN), was able to deliver siRNA to the cytoplasm and to knockdown gene expression up to 40% *in vitro* and 30% *in vivo*. We acknowledge that this knockdown is relatively modest and will require further improvement to reach levels of knockdown sufficient for therapeutic application. This study confirmed that functionalization of a cell penetrating peptide for siRNA delivery with an endosomal disruptor is an effective approach to target the cornea *in vivo.*  It also represents a valid proof-of-principle that can applied to safer and more effective endosomal disruptors [89](#_ENREF_89). Different treatment regimens and adjuvants that might increase the persistence of the drug on the eye surface may be tested as well, together with modified siRNAs having an increased resistance to nuclease degradation. The rational design presented in this study, combining an *in vitro* pre-screening with the *in vivo* assessment of therapeutic siRNA delivery and function in a corneal bioluminescence reporter mouse represents a methodology to evaluate the efficacy and topical delivery in the corneal epithelium.

# Materials and methods

2.1 Synthesis of peptides and preparation of nanoparticles

POD (CGGG[ARKKAAKA]4) [30] was modified in order to obtain: a Palmitoyl-POD (Palm-POD, MW 3829.9 g/mol), a Cholesteryl-POD (Chol-POD, MW 4004.1 g/mol) and a Quinoline-Palmitoyl-POD (QN-Palm-POD, MW 4873.0 g/mol) as described in Figure S1. The lipophilic derivatization was carried out in solid-phase at the N-terminus of the POD sequence. A fraction of the peptidyl-resin was treated with three-fold molar excesses of palmitic acid, N’, N’ diisopropylcarbodiimide and 1-hydroxybenzotriazole (HOBt) (all the reagents were from Fluka-Sigma-Aldrich, St. Louis, USA) in dimethylformamide (DMF) (Scharlau, Barcelona, Spain) at room temperature overnight.

Cholesterol was also conjugated at the N-terminus of another fraction of peptidyl resin. Modifications were introduced at the N-terminus of the Cell Penetrating Peptide (POD) in order to not alter/modify its secondary structure. The coupling took place by reaction of cholesteryl chloroformate (Fluka-Sigma-Aldrich, St. Louis, USA) (10 eq.) dissolved in dichloromethane (DCM) (Merck, KGaA, Darmstad, Germany), together with triethylamine (Fluka-Sigma-Aldrich, St. Louis, USA) (3 eq.) at room temperature overnight.

Both peptidyl-resins were treated with a mixture of 95% (v/v) trifluoroacetic acid (TFA) (Scharlau, Barcelona, Spain), 2% (v/v) MilliQ water, 1% (v/v) triisopropylsilane and 2% (v/v) β-mercaptoethanol (Fluka-Sigma-Aldrich, St. Louis, USA) for 3 hours at room temperature. The TFA was removed under N2 flow and the crude peptides were precipitated with diethyl ether (Merck, KGaA, Darmstad, Germany). The solids were dissolved in 30% (v/v) acetic acid (Panreac, AppliChem GmbH, Darmstad, Germany) in MilliQ water and lyophilized.

To obtain the Quinoline-Palmitoyl-POD, an N-α-9-fluorenylmethyloxycarbonyl-N-ε-4-methyltrityl-L-lysine (Fmoc-Lys(Mtt)-OH, 3 eq.) (Novabiochem, Merck Millipore, Merck, KGaA, Darmstad, Germany) amino acid derivative was coupled on solid phase to the N-terminus of the POD throughout activation with 2-(1H-7-azabenzotriazole-1-yl)-1,1,3,3-tetramethyluronium hexafluorophosphate methanaminium (HATU) (3 eq.) (Genscript, Piscataway, USA) and diisopropylethylamine (DIPEA) (6 eq.) (Fluka-Sigma-Aldrich, St. Louis, USA) in DMF. After removing the Fmoc protecting group by reaction with piperidine (Fluka-Sigma-Aldrich, St. Louis, USA) in DMF (20% v/v), the palmitic acid was coupled to the free N-α-amino group as described above. Subsequently, the methyltrityl protecting group of the N-Ɛ-amine of the lysine was selectively removed after repeated treatments with 1% TFA in DCM. A Fmoc-Lys(Fmoc)-OH (Novabiochem, Merck Millipore, Merck, KGaA, Darmstad, Germany) derivative was then incorporated through activation with HATU and DIPEA in DMF. Three-fold molar excess of reagents were used. The deprotection of the Fmoc group by repeated treatment with piperidine in DMF (20% v/v) rendered two free amino groups that were afterwards treated with succinic anhydride (Fluka-Sigma-Aldrich, St. Louis, USA) (1.5 eq.) and DIPEA (3 eq.) in DMF. The efficiency of the reactions was evaluated by the ninhydrin colorimetric test. The synthetic scheme of QN and of QN-Palm-POD are described in Figures S2 A and B.

In order to obtain the final Quinoline-Palm-POD derivative, the trifluoromethylquinoline derivative was first synthesized through reaction of 4-chloro-7-(trifluoromethyl)quinoline (Fluka-Sigma-Aldrich, St. Louis, USA) (16.4 mmol) and 2,2’-diamino-N-methyldiethylamine (TCI, Tokio, Japan) (194.1 mmol)[24]. The product, N-(2-aminoethyl)-N-methyl-N’-[7-(trifluoromethyl)-quinolin-4-yl]ethane-1,2-diamine (QN), was characterized by Matrix-assisted laser desorption/ionization time-of-flight mass spectrometry (MALDI-TOF) (Figure S2 C) and Proton Nuclear Magnetic Resonance (NMR-H+) (Figure S2 D). QN (2.5 eq.) was coupled overnight to the succinic acid modified peptidyl resin previously activated with 2-(1H-benzotriazole-1-yl)-1,1,3,3-tetramethylaminium tetrafluoroborate (TBTU) (Fluka-Sigma-Aldrich, St. Louis, USA) (3eq.), HOBt (3eq.) and DIPEA (6 eq.). Crude peptide was obtained after cleavage and final deprotection of the peptidyl-resin with TFA/water/β-mercaptoethanol/TIS (95/2/2/1).

The crude peptides were purified by semi-preparative HPLC (1260 Infinity, Agilent Technologies, Santa Clara, USA) in an XBridgeTM Prep BEH 130 C18 column (Waters, 5μm, 10x250 mm) at a flow rate of 3ml/min. The peptides were purified with a linear gradient of 5%-100% B (0.05% (v/v) TFA in acetonitrile) into A (0.05% (v/v) TFA in water) for 20 minutes. Their identity was confirmed by electrospray ionization mass spectrometry (ES-MS). Thus, purified peptides were characterized by an analytical ultra-performance liquid chromatograph (UPLC, Waters, Milford, MA, USA) coupled to a time of flight (LC-TOF) detector, LCT Premier XE (Micromass Waters, Milford, MA, USA). Samples were analysed in the UPLC at a flow rate of 0.3 ml/min. The mass spectra were recorded in positive ion mode in the m/z 500-2500 range. UPLC was performed in an Acquity UPLC BEH C18 reverse-phase column (2.1x100 mm, 1.7 μm particle size). Solvent A was 20 mM formic acid in acetonitrile and solvent B was 20 mM formic acid in water. Elution was performed with linear gradients of 5-100% A into B over 10 minutes. Figures S3 and S4in the Supplementary Material shows the characterization of the pure peptides by ES-MS and MALDI-TOF.

PLGA-PEG-POD-NPs were prepared by covalently binding POD to the pegylated polymer PLGA (poly(lactic-co-glycolic acid) as described in Figure S5. With this aim, PLGA was preactivated before PEGylation with maleimide-PEG-amine. The obtained PLGA-PEG copolymer was dried under vacuum and stored at 4°C. To conjugate the peptide with the PLGA-PEG-maleimide, POD was dissolved in acetonitrile/DMF and added to the polymer dissolved in chloroform. The mixture was covered tightly and stirred overnight. The product was precipitated with 3 ml of an ice-cold 80/20 mixture of diethyl ether/methanol, centrifuged at 2600 x g for 10 minutes, the supernatant discarded, and the product re-dissolved in 1 ml of chloroform. This cycle was repeated twice more and the purified PLGA-PEG-POD dried under vacuum.

1H-NMR was used to assess the grafting of PEG to PLGA and the conjugation with POD. The PLGA-PEG was dissolved in deuterated chloroform and the PLGA‐PEG‐POD in DMSO‐d6. The spectra were recorded at 298K on a Varian Inova 500 MHz spectrometer (Agilent Technologies, Santa Clara, USA). PLGA-PEG-POD NPs were prepared following the solvent displacement technique [29]. Briefly, an organic solution of the polymer containing the POD (PLGA-PEG-POD) in acetone was poured, with moderate stirring, into an RNase-free aqueous solution containing Poloxamer 188 (Lutrol F68). The resulting colloidal suspension was stirred for 5 minutes and the acetone was then evaporated and the NP dispersion was concentrated under reduced pressure. The mean particle size, polydispersity index (PI) and zeta potential were determined by dynamic light scattering (DLS) measurement using a Zetasizer nano ZS (Malvern Instruments, Malvern, UK) at 25ºC.

*2.2 Cell culture*

HCE-S, a spontaneously immortalised human corneal epithelial cell line (a gift from J.T. Daniels, Institute of Ophthalmology, University College London, UK) [50](#_ENREF_50), was grown in DMEM medium (GlutaMAX; Invitrogen, UK) supplemented with 10% Fetal Bovine Serum (FBS) (Thermo Fisher, UK). Cells were incubated under 5% CO2 at 37°C and passaged following standard laboratory procedures.

*2.3 Gel retardation assay*

To assess the formation of polyplexes between the siRNA and the PODs [90](#_ENREF_90), Chol-POD, Palm-POD, PEG-PLGA-POD and POD (Table 2) were mixed with siRNA in a PBS solution to give a final concentration of 35 M for the PODs and 1 M for the siRNA in a final volume of 10 l and incubated for 30 minutes at room temperature. These formulations were then analysed by electrophoresis on a 1% agarose, 0.5 x TBE (Tris-Borate-EDTA; UltraPure™ Agarose, Thermo Fisher, UK) gel for 40 minutes at 100 volts and the gel visualized using the Gel Logic 100 Imaging System (Kodak). To determine the optimal ratio for formation of polyplexes, the same procedure was repeated for the QN-Palm-POD at four different molar ratios (35:1, 70:1, 140:1 and 200:1 POD:siRNA).

*2.4 Measurement of dimension and* -*potential*

To measure the dimensions and the -potentials of the polyplexes, POD-siRNA formulations were prepared in a final volume of 50 l by mixing PODs and siRNA in PBS and incubated for 40 minutes at 25°C before analysis. For the measurement of particle size, a molar ratio of 140:1 for the QN-Palm-POD and 35:1 for all the other PODs was used. The samples were then diluted to 1 ml in distilled water before the measurement of zeta potential (the charge of the POD-siRNA polyplexes) using a Nano ZS Zetasizer and DTS software (Malvern Instruments, UK). Three measurements were collected for each sample and the values expressed as mean ± standard deviation.

*2.5 Measurement of effect of formulation upon cell viability (MTT assay)*

HCE-S cells were plated at a density of 1.5 x 104 cells/well in 96 well plates and transfected 24 hours later with POD-siRNA polyplexes at 17.5 M, 35 M and 70 M POD at 35:1 molar ratio in PBS, for Chol-, Palm- and POD and at 9 M, 17.5 M and 35 M POD at 140:1 molar ratio for the QN-Palm-POD. For each condition, n=5 replicates were tested. 24 h post-transfection, 0.5 mg/ml MTT reagent (Sigma-Aldrich, UK) was added to the media and the cells incubated for 2 h at 37°C, under 5% CO2. Absorbance was then measured at 570 nm and 650 nm in a plate reader (LUMIstar OPTIMA, BMG LABTECH, UK). The absorbance at 650 nm, subtracted from that at 570 nm, indicates cell viability, the results obtained were compared to an internal untreated control (maximum cell viability).

*2.6 In vitro fluorescence siRNA analysis with PODs-siRNA formulations*

Green fluorescent siRNA (siGLO, GE Dharmacon) was complexed with PODs and used to transfect HCE-S cells. Chol-, Palm- and POD were used at 35:1 molar ratio in PBS with 1 M green fluorescent siRNA, while QN-Palm-POD was used at 17.5 M with 0.125 M siGLO, for a final molar ratio of 140:1. HCE-S were seeded on coverslips at 105 cells/well in a 24 well plate, 24h before POD-siRNA transfection, and 24 hours after transfection, the coverslips were collected, fixed for 10 minutes in 4% paraformaldehyde in PBS (Thermo Scientific, USA) and mounted in Ultracruz Mounting media (Santa Cruz Biotechnology). Fluorescence was then assessed with an AxioScope A1 microscope equipped with a 20x/40x N Archoplan lens on an AxioCam MRc camera (Carl Zeiss, Germany).

To study the effect of endosomal disruptors on siRNA release, the experiment was repeated using the formulation at 35:1 molar ratio alone or in combination with 30 M Chlq (Sigma-Aldrich, UK) added 1 hour before transfection [41](#_ENREF_41).

*2.7 In vitro luciferase assay with POD-siLuc formulations*

A modified *in vitro* dual-luciferase assay was performed, as previously reported [26](#_ENREF_26),[56](#_ENREF_56), in which expression of Firefly luciferase, the siRNA target, is normalized to Renilla luciferase expression as an internal control of cell transfection: HCE-S cells were plated at 6.5 x 103 cells/well in a 96-well plate, transfected after 24 hours with the luciferase reporter plasmids and then treated 24 hours later with the different POD-siRNA formulations (1 M siRNA 35:1 POD:siRNA in a final volume of 100 l), using luciferase specific siRNA (siLuc, 5'- CGACAAGCCUGGCGCAGUAUU-3', with dTdT overhang at 3’ in both strands, Eurogentech, Belgium) and non-specific control siRNA (NSC4, 5′-UAGCGACUAAACACAUCAAUU-3′, inverted β-galactosidase sequence, with dTdT overhang at 3’ in both strands, Eurogentech, Belgium) [43](#_ENREF_43),[56](#_ENREF_56). Luciferase expression was measured 72 hours after POD-siRNA transfection and the values obtained expressed as a percentage of the luciferase activity measured with NSC4 (100%). The effect of Chlq upon knockdown of gene expression was investigated by transfecting cells with the POD-siRNA formulation, as above, along with 30 M Chlq, added 1 hour before transfection. As a positive control, cells were transfected with 1 M siLuc/NSC4 siRNA complexed with RNAiMAX (Thermo Fisher, Invitrogen, UK) as previously described [91](#_ENREF_91). The experiment was further repeated with QN-Palm-POD at a 140:1 ratio and with QN-Palm-POD in combination with free Chlq.

*2.8 Live animal imaging*

Animals were used for the following experiments in accordance with the UK Animal Welfare Act; the experiments were approved by the Home Office (Scotland) and the DHSSPS (Northern Ireland). The experiments to assess delivery of fluorescent siRNA (siGLO) to the cornea were performed on wild-type C57BL/6 mice. To assess functionality of the delivered siRNA we used a transgenic mouse line expressing luciferase in the cornea epithelium. This animal model was developed by inserting a synthetic multi-target cassette composed of Meesmann epithelial corneal dystrophy-causing mutations (L132P and R135T in keratin 12 and E509K, R503P, and E498V in keratin 3 [92](#_ENREF_92),[93](#_ENREF_93)) with 40 base pair flanking regions into the 3’UTR of the firefly luciferase reporter gene *luc2* (codon-optimized for mammalian expression) under the control of the endogenous *Krt12* promoter on a C57BL/6 background. Mice were genotyped by extracting genomic DNA (gDNA) from ear biopsies by standard protocols. A common reverse primer was used (K12KI.R): 5’-TGAACGGAACTGTACTTCTGTG-3’ with primers K12KI.2F: 5’-ACGTCCAGACACAGCATAGG-3’ and K12KI.1F: 5’-GCTGTGGAGGCCTCTTTTC-3’) in equimolar concentrations, in order to detect either the luciferase knock-in allele with a 299bp product or the the WT allele with a 553bp product (Figure S6).

For live imaging, mice between 12 and 25 weeks old were anaesthetised using 1.5-2% isoflurane in oxygen (Abbott Laboratories Ltd., Berkshire, UK) at a flow rate of ~1.5 l/min. To measure luciferase reporter gene expression, luciferin substrate (30 mg/ml D-luciferin potassium salt; Gold Biotechnology, St. Louis, USA) mixed 1:1 w/v with Viscotears gel (Novartis, Camberley, UK) was applied to the eye of heterozygous luc2 transgenic mice 1 minute prior to imaging. A Xenogen IVIS Lumina (Perkin Elmer, Cambridge, UK) was used to quantify luminescence and fluorescence. In each mouse eye a region of interest (ROI) was selected for quantification. ROIs parameters (size and shape) were kept constant throughout, using protocols as previously described [62](#_ENREF_62).

*2.9 Intrastromal injection*

Intrastromal injection of Accell siRNA was performed by a trained ophthalmic surgeon as previously described [65](#_ENREF_65). 2 µl of 150 pmol/µl Cy3-labelled Accell-modified siRNA were injected intrastromally in to the right eyes of WT C57BL/6J mice. To assess the persistence of Cy3-labelled siRNA, animals were imaged on the Xenogen IVIS Lumina system at 0, 6, 24, 48 and 72 hours post-injection (n=3). Mice were sacrificed at 0, 6 and 12 hours after injection (n=3), eyes were enucleated and frozen at -80°C. Tissue was fixed in OCT and cryosectioned for fluorescence microscopy. To assess luciferase knock down mice were treated in a split body control (untreated vs Accell-siRNA and untreated vs Acell-NSC4) for 7 days after the treatment (n=3). Luciferase signal was quantified as described in section 2.8. Baseline luciferase reporter gene expression (day 0) was a mean value obtained by measurement of ocular luminescence daily, for three days before treatment.

*2.10 In vivo POD-siRNA studies*

Mice between 12 and 25 weeks old were anaesthetised using 1.5-2% isoflurane in air (Abbott Laboratories Ltd., Berkshire, UK) at a flow rate of ~1.5 l/min. Formulations containing 35:1 molar ratio POD:siRNA (Chol- and Palm-), with 18 M siRNA and 625 M POD or QN-Palm-POD:siRNA at a 140:1 molar ratio with 5 M siRNA, in a total volume of 2.5 l of PBS per eye were prepared, incubated at room temperature for 30 minutes and then applied as a drop to the cornea of anesthetized mice which were maintained with the eye in a horizontal position. After application, the mouse was kept anesthetized for a further 15 minutes, over which period the droplet was observed to remain on the eye, to allow absorption and maximize uptake. Following treatment, fluorescence and luciferase experiments were performed as described:

 *2.10.1 Assessment of siRNA uptake by in vivo fluorescence assay*

To assess the uptake of siRNA by the corneal epithelium*, in vivo* fluorescence assays were performed by treating wild-type mice (n=2 for each condition). 100 M red siGLO (# D-001630-02, GE Dharmacon) was used in combination with Chol- or Palm-POD. The siRNA-POD polyplexes were applied to the right eye while siGLO alone was applied to the left eye of each mouse as control. Measurements were obtained from two untreated mice to determine background fluorescence. Fluorescence was detected with a Xenogen IVIS with LivingImage 3.2 software (both Perkin Elmer, Cambridge, UK) using DS Red filters (Ex. 570 nm Em. 620 nm) at 3, 6, 24 hours following application. Fluorescence was quantified after selecting a region of interest (ROI) tightly cropped to the fluorescent regions in the eyes and the ROI was kept constant in all subsequent measurements. After the final measurement, mice were sacrificed, the eyes enucleated, fixed in 4% paraformaldehyde (prepared in PBS, pH 7.4) for 30 minutes at room temperature, submerged in Poly-Freeze (P0091 SIGMA, Sigma-Aldrich) and immediately frozen at -80°C. 5 m sections were cut with a cryostat (CM 1850, Leica), mounted on 3-Aminopropyltriethoxysilane (APES) (Sigma Aldrich, UK) coated slides, treated with a mounting medium containing 4’,6’-diamidino-2-phenylindole (DAPI) (DAPI I, Vysis Inc, USA), to stain the nuclei, and fluorescence was visualized with a fluorescence microscope (as described above).

 *2.10.2 Assessment of siRNA-mediated gene expression knockdown by in vivo luciferase expression analysis*

*In vivo* luciferase experiments were performed using a split body control by comparing the treatment under test, in one eye, with a negative control in the other eye of the same animal: the right eye was treated with QN-Palm-POD and NSC4 while the left one with QN-Palm-POD and siLuc. QN-Palm-POD:siRNA were at a 140:1 molar ratio with 5 M siRNA. Experiments and treatment were performed in n=4 mice. Baseline luciferase reporter gene expression was determined by measurement of ocular luminescence daily for three days before treatment. Ocular luminescence was measured before POD-siRNA complexes were applied daily, as described above, for four days and ocular luminescence was then measured daily for a further 4 days after cessation of treatment.

 *2.10.3 Hematoxylin and eosin staining of the mouse cornea*

After the final measurement of luminescence, mice were sacrificed and eyes enucleated, paraformaldehyde fixed, dehydrated through graduated ethanol solutions and paraffin embedded. 5 m sections were obtained using a microtome (Leica RM 2135), mounted on 3-Aminopropyltriethoxysilane (APES) (Sigma Aldrich, UK) coated slides, dewaxed and rehydrated and stained with hematoxylin and eosin solution (both from Sigma-Aldrich, UK). Sections were visualized using an AxioScope A1 microscope as described previously.

*2.11 Statistical Analysis*

Statistical analysis was performed using Microsoft Excel 2010 and GraphPad Prism 5 software. Data were presented as mean±standard error of the mean (SEM). The different treatment groups were compared using two-tailed student's t-test and analysis of variance. For *in vitro* assays, a student’s t-test was performed upon treatment groups composed of n=5 replicates. Significance was set at p<0.05. For the *in vivo* POD luciferase experiments, the statistical comparison was done by comparing the average right:left ratio for 5 mice in the first 3 days before the beginning of the treatment with the ratios measured on each of the single days after the beginning of the treatment.

# Acknowledgements

This work was supported by the United Kingdom Fight for Sight grant (C.B.T.M.), The Belfast Association for the Blind (S.D.A., M.A.N. and C.B.T.M.) and Northern Ireland Clinical Research Network Vision Research Translation Research Group (M.A.N. and C.B.T.M.). Partial financial support from the Spanish Ministry of Economy, Industry and Competitiveness (MINECO) and the European Regional Development Fund (Grant CTQ2015-63919-R)(I.H.) is also gratefully acknowledged.

**Author Contributions**

D.S., T.M., M.A.N and I.H. conceived of and designed the experiments. D.S, M.J.G., E.M., S.D.A, L.M., K.A.C., D.F.C. and C.M.M. performed the experiments. D.S., E.M., S.D.A, T.M. and I.H. analyzed the data. D.S., E.M., M.A.N. and T.M. wrote the paper.

**References**

1 Guzman‐Aranguez, A., Loma, P. & Pintor, J. Small‐interfering RNAs (siRNAs) as a promising tool for ocular therapy. *British journal of pharmacology* **170**, 730-747 (2013).

2 Bobbin, M. L. & Rossi, J. J. RNA Interference (RNAi)-Based Therapeutics: Delivering on the Promise? *Annual review of pharmacology and toxicology* **56**, 103-122, doi:10.1146/annurev-pharmtox-010715-103633 (2016).

3 Yavuz, B. & Kompella, U. B. in *Pharmacologic Therapy of Ocular Disease* 57-93 (Springer, 2016).

4 Järvinen, K., Järvinen, T. & Urtti, A. Ocular absorption following topical delivery. *Advanced drug delivery reviews* **16**, 3-19 (1995).

5 Subrizi, A. *et al.* Design principles of ocular drug delivery systems: importance of drug payload, release rate, and material properties. *Drug discovery today* (2019).

6 Kim, Y. C., Chiang, B., Wu, X. & Prausnitz, M. R. Ocular delivery of macromolecules. *Journal of Controlled Release* **190**, 172-181 (2014).

7 Urtti, A. Challenges and obstacles of ocular pharmacokinetics and drug delivery. *Advanced drug delivery reviews* **58**, 1131-1135 (2006).

8 Berdugo, M. *et al.* Delivery of antisense oligonucleotide to the cornea by iontophoresis. *Antisense and Nucleic Acid Drug Development* **13**, 107-114 (2003).

9 Eljarrat-Binstock, E. & Domb, A. J. Iontophoresis: a non-invasive ocular drug delivery. *Journal of Controlled Release* **110**, 479-489 (2006).

10 Hao, J., Li, S. K., Liu, C.-Y. & Kao, W. W. Electrically assisted delivery of macromolecules into the corneal epithelium. *Experimental eye research* **89**, 934-941 (2009).

11 Li, Z., Duan, F., Lin, L., Huang, Q. & Wu, K. A new approach of delivering siRNA to the cornea and its application for inhibiting herpes simplex keratitis. *Current molecular medicine* **14**, 1215-1225 (2014).

12 Souza, J. G., Dias, K., Pereira, T. A., Bernardi, D. S. & Lopez, R. F. Topical delivery of ocular therapeutics: carrier systems and physical methods. *Journal of Pharmacy and Pharmacology* **66**, 507-530 (2014).

13 Solinís, M. Á., del Pozo-Rodríguez, A., Apaolaza, P. S. & Rodríguez-Gascón, A. Treatment of ocular disorders by gene therapy. *European Journal of Pharmaceutics and Biopharmaceutics* **95**, 331-342 (2015).

14 Williams, K. A. & Irani, Y. D. Gene Therapy and Gene Editing for the Corneal Dystrophies. *The Asia-Pacific Journal of Ophthalmology* **5**, 312-316 (2016).

15 Mohan, R. R., Rodier, J. T. & Sharma, A. Corneal gene therapy: basic science and translational perspective. *The ocular surface* **11**, 150-164 (2013).

16 Ozcan, G., Ozpolat, B., Coleman, R. L., Sood, A. K. & Lopez-Berestein, G. Preclinical and clinical development of siRNA-based therapeutics. *Advanced drug delivery reviews* **87**, 108-119 (2015).

17 Klintworth, G. K. Corneal dystrophies. *Orphanet journal of rare diseases* **4**, 7 (2009).

18 Weiss, J. S. *et al.* IC3D classification of corneal dystrophies—edition 2. *Cornea* **34**, 117-159 (2015).

19 Allen, E. H. *et al.* Keratin 12 missense mutation induces the unfolded protein response and apoptosis in Meesmann epithelial corneal dystrophy. *Human molecular genetics*, ddw001 (2016).

20 Courtney, D. G. *et al.* siRNA Silencing of the Mutant Keratin 12 Allele in Corneal Limbal Epithelial Cells Grown From Patients With Meesmann's Epithelial Corneal DystrophysiRNA Silencing of Mutant Keratin 12 Allele. *Investigative ophthalmology & visual science* **55**, 3352-3360 (2014).

21 Courtney, D. G. *et al.* Development of Allele-Specific Gene-Silencing siRNAs for TGFBI Arg124Cys in Lattice Corneal Dystrophy Type IAllele-Specific Gene-Silencing siRNAs. *Investigative ophthalmology & visual science* **55**, 977-985 (2014).

22 Liao, H. *et al.* Development of allele-specific therapeutic siRNA in Meesmann epithelial corneal dystrophy. *PloS one* **6**, e28582-e28582 (2011).

23 McLean, W. I. & Moore, C. T. Keratin disorders: from gene to therapy. *Human molecular genetics* **20**, R189-R197 (2011).

24 Unniyampurath, U., Pilankatta, R. & Krishnan, M. N. RNA Interference in the Age of CRISPR: Will CRISPR Interfere with RNAi? *International journal of molecular sciences* **17**, 291 (2016).

25 Boettcher, M. & McManus, M. T. Choosing the right tool for the job: RNAi, TALEN, or CRISPR. *Molecular cell* **58**, 575-585 (2015).

26 Atkinson, S. D. *et al.* Development of allele-specific therapeutic siRNA for keratin 5 mutations in epidermolysis bullosa simplex. *Journal of Investigative Dermatology* **131**, 2079-2086 (2011).

27 Hickerson, R. P. *et al.* Single-nucleotide-specific siRNA targeting in a dominant-negative skin model. *Journal of Investigative Dermatology* **128**, 594-605 (2008).

28 Wilkes, R. P., Ward, D. A., Newkirk, K. M., Adams, J. K. & Kania, S. A. Evaluation of delivery agents used for introduction of small interfering RNAs into feline corneal cells. *American journal of veterinary research* **74**, 243-247 (2013).

29 Rabinovich-Guilatt, L., Couvreur, P., Lambert, G. & Dubernet, C. Cationic vectors in ocular drug delivery. *Journal of drug targeting* **12**, 623-633 (2004).

30 Patel, A., Cholkar, K., Agrahari, V. & Mitra, A. K. Ocular drug delivery systems: an overview. *World journal of pharmacology* **2**, 47 (2013).

31 Zhang, S., Zhao, B., Jiang, H., Wang, B. & Ma, B. Cationic lipids and polymers mediated vectors for delivery of siRNA. *Journal of Controlled Release* **123**, 1-10 (2007).

32 Calvo, P., Vila-Jato, J. L. & Alonso, M. a. J. Evaluation of cationic polymer-coated nanocapsules as ocular drug carriers. *International Journal of Pharmaceutics* **153**, 41-50 (1997).

33 Lindgren, M. & Langel, Ü. Classes and prediction of cell-penetrating peptides. *Cell-Penetrating Peptides: Methods and Protocols*, 3-19 (2011).

34 Kurrikoff, K., Gestin, M. & Langel, U. Recent in vivo advances in cell-penetrating peptide-assisted drug delivery. *Expert Opin Drug Deliv* **13**, 373-387, doi:10.1517/17425247.2016.1125879 (2016).

35 Endoh, T. & Ohtsuki, T. Cellular siRNA delivery using cell-penetrating peptides modified for endosomal escape. *Advanced drug delivery reviews* **61**, 704-709 (2009).

36 Juliano, R. L. The delivery of therapeutic oligonucleotides. *Nucleic acids research*, gkw236 (2016).

37 Vasconcelos, A. C. *et al.* Conjugation of cell-penetrating peptides with poly (lactic-co-glycolic acid)-polyethylene glycol nanoparticles improves ocular drug delivery. (2015).

38 Johnson, L. N., Cashman, S. M. & Kumar-Singh, R. Cell-penetrating peptide for enhanced delivery of nucleic acids and drugs to ocular tissues including retina and cornea. *Molecular Therapy* **16**, 107-114 (2008).

39 Pescina, S. *et al.* Design and synthesis of new cell penetrating peptides: diffusion and distribution inside the cornea. *Molecular pharmaceutics* **13**, 3876-3883 (2016).

40 Bouheraoua, N., Jouve, L., Borderie, V. & Laroche, L. Three Different Protocols of Corneal Collagen Crosslinking in Keratoconus: Conventional, Accelerated and Iontophoresis. *Journal of visualized experiments : JoVE*, doi:10.3791/53119 (2015).

41 Bhattarai, S. R. *et al.* Enhanced gene and siRNA delivery by polycation-modified mesoporous silica nanoparticles loaded with chloroquine. *Pharmaceutical research* **27**, 2556-2568 (2010).

42 Gebhart, C. L. & Kabanov, A. V. Evaluation of polyplexes as gene transfer agents. *Journal of Controlled Release* **73**, 401-416 (2001).

43 Allen, E. H. *et al.* Allele-Specific siRNA Silencing for the Common Keratin 12 Founder Mutation in Meesmann Epithelial Corneal DystrophyAllele-Specific siRNA Silencing. *Investigative ophthalmology & visual science* **54**, 494-502 (2013).

44 Jing, X. *et al.* Delivery of siRNA Complexed with Palmitoylated α-Peptide/β-Peptoid Cell-Penetrating Peptidomimetics: Membrane Interaction and Structural Characterization of a Lipid-Based Nanocarrier System. *Molecular pharmaceutics* **13**, 1739-1749 (2016).

45 Qin, B., Chen, Z., Jin, W. & Cheng, K. Development of cholesteryl peptide micelles for siRNA delivery. *Journal of Controlled Release* **172**, 159-168 (2013).

46 Binder, C., Cashman, S. M. & Kumar-Singh, R. Extended duration of transgene expression from pegylated POD nanoparticles enables attenuation of photoreceptor degeneration. *PloS one* **8**, e82295 (2013).

47 van Asbeck, A. H. *et al.* Molecular parameters of siRNA–cell penetrating peptide nanocomplexes for efficient cellular delivery. *ACS nano* **7**, 3797-3807 (2013).

48 Kim, S. W. *et al.* RNA interference in vitro and in vivo using an arginine peptide/siRNA complex system. *Journal of Controlled Release* **143**, 335-343 (2010).

49 Hatakeyama, H. *et al.* A pH-sensitive fusogenic peptide facilitates endosomal escape and greatly enhances the gene silencing of siRNA-containing nanoparticles in vitro and in vivo. *Journal of Controlled Release* **139**, 127-132 (2009).

50 Notara, M. & Daniels, J. T. Characterisation and functional features of a spontaneously immortalised human corneal epithelial cell line with progenitor-like characteristics. *Brain research bulletin* **81**, 279-286 (2010).

51 Greco, D. *et al.* Gene expression analysis in SV-40 immortalized human corneal epithelial cells cultured with an air-liquid interface. *Molecular vision* **16**, 2109 (2010).

52 Toropainen, E., Hornof, M., Kaarniranta, K., Johansson, P. & Urtti, A. Corneal epithelium as a platform for secretion of transgene products after transfection with liposomal gene eyedrops. *The Journal of Gene Medicine: A cross‐disciplinary journal for research on the science of gene transfer and its clinical applications* **9**, 208-216 (2007).

53 Rönkkö, S., Vellonen, K.-S., Järvinen, K., Toropainen, E. & Urtti, A. Human corneal cell culture models for drug toxicity studies. *Drug delivery and translational research* **6**, 660-675 (2016).

54 El‐Andaloussi, S., Johansson, H. J., Lundberg, P. & Langel, Ü. Induction of splice correction by cell‐penetrating peptide nucleic acids. *The journal of gene medicine* **8**, 1262-1273 (2006).

55 Chiu, Y.-L., Ali, A., Chu, C.-y., Cao, H. & Rana, T. M. Visualizing a correlation between siRNA localization, cellular uptake, and RNAi in living cells. *Chemistry & biology* **11**, 1165-1175 (2004).

56 Liao, H. *et al.* Development of allele-specific therapeutic siRNA in Meesmann epithelial corneal dystrophy. *PloS one* **6**, e28582 (2011).

57 Erazo-Oliveras, A., Muthukrishnan, N., Baker, R., Wang, T.-Y. & Pellois, J.-P. Improving the endosomal escape of cell-penetrating peptides and their cargos: strategies and challenges. *Pharmaceuticals* **5**, 1177-1209 (2012).

58 Ma, D. Enhancing endosomal escape for nanoparticle mediated siRNA delivery. *Nanoscale* **6**, 6415-6425 (2014).

59 Varkouhi, A. K., Scholte, M., Storm, G. & Haisma, H. J. Endosomal escape pathways for delivery of biologicals. *Journal of Controlled Release* **151**, 220-228 (2011).

60 Pedrioli, D. M. L. *et al.* Generic and personalized RNAi-based therapeutics for a dominant-negative epidermal fragility disorder. *Journal of Investigative Dermatology* **132**, 1627-1635 (2012).

61 Smith, F. J. *et al.* Development of therapeutic siRNAs for pachyonychia congenita. *Journal of investigative dermatology* **128**, 50-58 (2008).

62 Hegde, V. *et al.* In vivo gene silencing following non-invasive siRNA delivery into the skin using a novel topical formulation. *Journal of Controlled Release* **196**, 355-362 (2014).

63 Leachman, S. A. *et al.* Therapeutic siRNAs for dominant genetic skin disorders including pachyonychia congenita. *Journal of dermatological science* **51**, 151-157 (2008).

64 Moore, J. E. *et al.* The inflammatory milieu associated with conjunctivalized cornea and its alteration with IL-1 RA gene therapy. *Investigative ophthalmology & visual science* **43**, 2905-2915 (2002).

65 Courtney, D. *et al.* CRISPR/Cas9 DNA cleavage at SNP-derived PAM enables both in vitro and in vivo KRT12 mutation-specific targeting. *Gene therapy* **23**, 108 (2016).

66 Bernstein, H. Chloroquine ocular toxicity. *Survey of ophthalmology* **12**, 415 (1967).

67 Andaloussi, S. E. *et al.* Design of a peptide-based vector, PepFect6, for efficient delivery of siRNA in cell culture and systemically in vivo. *Nucleic Acids Res* **39**, 3972-3987, doi:10.1093/nar/gkq1299 (2011).

68 Wittrup, A. & Lieberman, J. Knocking down disease: a progress report on siRNA therapeutics. *Nature Reviews Genetics* **16**, 543 (2015).

69 Liang, S. Y.-W. & Lee, G. A. Intrastromal injection of antibiotic agent in the management of recalcitrant bacterial keratitis. *Journal of Cataract & Refractive Surgery* **37**, 960-962 (2011).

70 Liu, C. *et al.* Facile noninvasive retinal gene delivery enabled by penetratin. *ACS applied materials & interfaces* **8**, 19256-19267 (2016).

71 Arukuusk, P., Pärnaste, L., Hällbrink, M. & Langel, Ü. PepFects and NickFects for the intracellular delivery of nucleic acids. *Cell-Penetrating Peptides: Methods and Protocols*, 303-315 (2015).

72 Hou, K. K., Pan, H., Schlesinger, P. H. & Wickline, S. A. A role for peptides in overcoming endosomal entrapment in sirna delivery—A focus on melittin. *Biotechnology advances* **33**, 931-940 (2015).

73 Pae, J. & Pooga, M. Peptide-mediated delivery: an overview of pathways for efficient internalization. *Therapeutic delivery* **5**, 1203-1222 (2014).

74 Reissmann, S. Cell penetration: scope and limitations by the application of cell‐penetrating peptides. *Journal of Peptide Science* **20**, 760-784 (2014).

75 Fonseca, S. B., Pereira, M. P. & Kelley, S. O. Recent advances in the use of cell-penetrating peptides for medical and biological applications. *Advanced drug delivery reviews* **61**, 953-964 (2009).

76 Vivès, E., Schmidt, J. & Pèlegrin, A. Cell-penetrating and cell-targeting peptides in drug delivery. *Biochimica et Biophysica Acta (BBA)-Reviews on Cancer* **1786**, 126-138 (2008).

77 Read, S. P., Cashman, S. M. & Kumar‐Singh, R. A poly (ethylene) glycolylated peptide for ocular delivery compacts DNA into nanoparticles for gene delivery to post‐mitotic tissues in vivo. *The journal of gene medicine* **12**, 86-96 (2010).

78 Read, S. P., Cashman, S. M. & Kumar-Singh, R. POD nanoparticles expressing GDNF provide structural and functional rescue of light-induced retinal degeneration in an adult mouse. *Molecular Therapy* **18**, 1917-1926 (2010).

79 Tiemann, K. & Rossi, J. J. RNAi‐based therapeutics–current status, challenges and prospects. *EMBO molecular medicine* **1**, 142-151 (2009).

80 Rojo, N., Gomara, M., Haro, I. & Alsina, M. Lipophilic derivatization of synthetic peptides belonging to NS3 and E2 proteins of GB virus‐C (hepatitis G virus) and its effect on the interaction with model lipid membranes. *Chemical Biology & Drug Design* **61**, 318-330 (2003).

81 Pérez-López, S. *et al.* Interaction of GB virus C/hepatitis G virus synthetic peptides with lipid langmuir monolayers and large unilamellar vesicles. *The Journal of Physical Chemistry B* **113**, 319-327 (2008).

82 McCarthy, H. O. *et al.* Development and characterization of self-assembling nanoparticles using a bio-inspired amphipathic peptide for gene delivery. *Journal of Controlled Release* **189**, 141-149, doi:<http://doi.org/10.1016/j.jconrel.2014.06.048> (2014).

83 El-Sayed, A., Futaki, S. & Harashima, H. Delivery of macromolecules using arginine-rich cell-penetrating peptides: ways to overcome endosomal entrapment. *The AAPS journal* **11**, 13-22 (2009).

84 Sánchez-López, E., Espina, M., Doktorovova, S., Souto, E. & García, M. Lipid nanoparticles (SLN, NLC): overcoming the anatomical and physiological barriers of the eye–part I–barriers and determining factors in ocular delivery. *European Journal of Pharmaceutics and Biopharmaceutics* **110**, 70-75 (2017).

85 Taketani, Y. *et al.* Topical Use of Angiopoietin-like Protein 2 RNAi-loaded Lipid Nanoparticles Suppresses Corneal Neovascularization. *Molecular Therapy - Nucleic Acids* **5**, e292, doi:https://doi.org/10.1038/mtna.2016.1 (2016).

86 Urgard, E. *et al.* Pre-administration of PepFect6-microRNA-146a nanocomplexes inhibits inflammatory responses in keratinocytes and in a mouse model of irritant contact dermatitis. *Journal of Controlled Release* **235**, 195-204, doi:<http://doi.org/10.1016/j.jconrel.2016.06.006> (2016).

87 Suhorutsenko, J. *et al.* Cell-penetrating peptides, PepFects, show no evidence of toxicity and immunogenicity in vitro and in vivo. *Bioconjugate chemistry* **22**, 2255-2262 (2011).

88 Anko, M. *et al.* Influence of stearyl and trifluoromethylquinoline modifications of the cell penetrating peptide TP10 on its interaction with a lipid membrane. *Biochimica et Biophysica Acta (BBA)-Biomembranes* **1818**, 915-924 (2012).

89 Joris, F. *et al.* Repurposing cationic amphiphilic drugs as adjuvants to induce lysosomal siRNA escape in nanogel transfected cells. *Journal of controlled release : official journal of the Controlled Release Society* **269**, 266-276, doi:10.1016/j.jconrel.2017.11.019 (2018).

90 Gary, D. J. *et al.* Influence of nano-carrier architecture on in vitro siRNA delivery performance and in vivo biodistribution: polyplexes vs micelleplexes. *ACS nano* **5**, 3493-3505, doi:10.1021/nn102540y (2011).

91 Maurizi, E. *et al.* A novel role for CRIM1 in the corneal response to UV and pterygium development. *Experimental eye research* (2018).

92 Kao, W. *et al.* Keratin 12-deficient mice have fragile corneal epithelia. *Investigative ophthalmology & visual science* **37**, 2572-2584 (1996).

93 Irvine, A. D. *et al.* Mutations in cornea-specific keratin K3 or K12 genes cause Meesmann's corneal dystrophy. *Nature genetics* **16**, 184-187 (1997).

**Figure Legends**

**Figure 1. Palm-POD and Chol-POD encapsulate siRNA and penetrate into HCE-S cells.**

(A) Gel retardation assay showing uncomplexed siRNA (arrow, siRNA only) migrated through the agarose gel, while the siRNA complexed with the PODs remained immobilized within the wells. 1 M siRNA was complexed with: Chol-POD, Palm-POD, PLGA-PEG-POD and POD (35 M) to a final molar ratio of 35:1 POD:siRNA. (B) Fluorescence images of HCE-S cells collected 24 hours after transfection with 1 M green siGLO and: Chol-POD, Palm-POD, PLGA-PEG-POD and POD at 35:1 molar ratio. Transfection with RNAiMAX and 1 M green siGLO was used as positive control while 1 M green siGLO only as negative control. The nuclei are stained with DAPI (Blue), while the green dots represent green siGLO. (C) MTT cell viability assay was performed on HCE-S at 24 hours after treatment with different concentrations of PODs-siRNA. Chol-, Palm- , PLGA-PEG-POD and POD were used at 17.5, 35 and 70 M (dark grey bars) and complexed with siRNA at 35:1 molar ratio. Untreated control (light grey bar) is represented on the right. (D) Dual luciferase reporter gene expression assay was performed *in vitro*: luminescence was measured 72 hours after treating HCE-S cells with POD-siRNA (35:1 molar ratio, 1 M siRNA). Black bars represent the luciferase activity in the siLuc transfected wells, while the grey bars the luciferase in the NSC4 transfected wells. The mean values of the NSC4 were normalized to 100% and the siLuc mean values expressed as a percentage of the negative control. A positive control with RNAiMAX and 1 M siLuc was also assessed (\*\*\*= p < 0.001). Error bars = standard error of the mean, n=4 biological replicates.

**Figure 2. Chlq addition to PODs disrupts endosomes, promotes siRNA release and luciferase knockdown.**

(A) Fluorescence images of HCE-S cells 24 hours after transfection with 1 M green siGLO and:Chol-POD, Palm-POD, PLGA-PEG-POD and POD with Chlq. The nuclei are stained with DAPI (Blue), while the green dots represent green siGLO. Scale bar 25M. (B) Dual luciferase reporter gene expression assays were performed as described above. HCE-S cells were treated with a 35:1 molar ratio (POD:siRNA) and Chlq and luminescence was measured 72 hours later. Black bars represent the luciferase activity in the siLuc transfected wells, and the grey bars the NSC4 siRNA transfected wells. \* = p<0.05, \*\* = p<0.01, \*\*\* = p<0.001). Error bars = standard error of the mean, n=4 biological replicates. A positive control with RNAiMAX and 1 M siLuc was also assessed.

**Figure 3.** ***In vivo* intrastromal injection of Accell Cy3-labelled siRNA efficiently knocked down luciferase expression**.

(A) Fluorescent images of a live mouse at time points following intrastromal injection of Cy3-labelled Accell siRNA showing strongest fluorescent signal at 0 and 6 hours post- injection, with a readily detectable signal still evident at 48 hours. (B) Fluorescence microscopy of transverse mice corneal sections shows that the siRNA (red) is well distributed and strongly accumulates in the anterior epithelium by 6 hours post- injection. By 12 hours post-injection, the signal has diminished, however, there is still a prominent Cy3 signal in the epithelium, which is more clearly seen within the inset portion of the image where the blue DAPI channel has been masked. E = epithelium; S = stroma. Scale bar = 150µm. (C)*In vivo* gene inhibition by intrastromal injection of luc2 siRNA. Representative images of animals (n=3 per group) imaged over 7 days. Left eyes were untreated. Right eyes were treated with a single intrastromal injection of Accell- modified siRNA after imaging on day 0. NSC4 = nonspecific control siRNA; siLuc = luciferase-specific siRNA). (D) Quantification of luciferase activity for each treatment group expressed as a percentage of control (R/L ratio %). Inhibition of luciferase with siLuc was sustained through days 2 to 7. NSC4 had no effect.

**Figure 4. *In vivo* topical application of Chol- and Palm-POD showed corneal delivery of siGLO**

(A) Comparison between wild-type mice treated with Chol- and Palm-POD combined with red siGLO (right eye) and siGLO alone (left eye, negative control). The images were collected at 3, 6 and 24 hours after treatment with IVIS Xenogen. The red and yellow colour represents the intensity of the fluorescence and not the colour of the siGlo signal. (B) Fluorescence measurements of the treated eye at the different conditions reported in A) Palm-POD demonstrated a significant increase in the fluorescent signal either at 3 and 6 hours after treatment when compared with Chol-POD and siGlo only. The values represent the mean (and the standard errors) of two treated eyes in n=2 mice. (C) Corneal sections of the eyes collected from the treated mice at 24 hours with either Chol- or Palm-POD and siGLO. The nuclei are stained blue (DAPI) while the siGLO is red in all images. Fluorescence is present in eyes treated with both Chol- and Palm-POD while no red fluorescence distinguishable from the background is visible in the negative control (siGLO only)**.** E and S indicate corneal epithelium and stroma, respectively.

**Figure 5. *In vitro* characterization of QN-Palm-POD-siRNA**

(A) QN-Palm-POD with the amino acidic chain, the palmitoyl group and QN group, the chemical structure of which is shown in detail. (B) Gel retardation assay of QN-Palm-POD complexed with 1 M siRNA at 35:1, 70:1, 140:1 and 200:1 molar ratios. The siRNA alone (siRNA only) migrated through the agarose gel, while the siRNA complexed with the PODs remained immobilized within the wells, either partially (35:1 and 70:1) or completely (140:1 and 200:1). (C) MTT assay performed on HCE-S treated with siRNA and QN-Palm-PODs 24 hours after the treatment. POD was used at 8.75 17.5 and 35 M (dark grey bars) at a 140:1 molar ratio. Untreated control (light grey bar). (D) Fluorescence image of HCE-S cells 24 hours after transfection with 1 M green siGLO (green) and QN-Palm-POD. The nuclei are stained with DAPI (Blue), scale bar 25M. (E) In dual luciferase reporter gene expression assays HCE-S cells were treated with a 35:1 molar ratio (QN-Palm-POD:siRNA) and luminescence was measured 72 hours later. Black bars represent the luciferase activity in the siLuc transfected wells, and the grey bars the NSC4 siRNA transfected wells. \* = p<0.05, \*\* = p<0.01, \*\*\* = p<0.001). Error bars = standard error of the mean, n=4 biological replicates. A positive control with RNAiMAX and 1 M siLuc was also assessed.

**Figure 6. *In vivo* topical application of siRNA with QN-PALM-POD demonstrated efficient delivery and knockdown in cornea**

(A) *In vivo* comparison of wild-type mice treated with QN-Palm-POD and red siGLO with and without AmB. The formulation was applied to the right eye while siGLO alone was applied to the left eye (negative control). The images were collected with IVIS Xenogen at 3, 6 and 24 hours after treatment. The red and yellow colour represents the intensity of the fluorescence and not the colour of the fluorescent signal. (B) Fluorescence measurements of the treated eye at the different conditions reported in (A). The values represent the mean (and the standard errors) of two treated eyes in n=2 mice. (C) Corneal sections of the eyes collected from the treated mice at 24 hours reported in (A). The nuclei are stained with DAPI (blue), while the red fluorescence represents siGLO. Fluorescence is present in eyes treated with QN-Palm-POD in all the layers of the cornea.

(D) Representative daily images of one of the four mice during the treatment (10 days) with siLuc and QN-palm-POD in the right eye and with NSC4 and QN-Palm-POD in the left eye. (E) Quantification of luciferase activity for a treatment group (n=4) expressed as a percentage of the right eye/left eye ratio (R/L ratio %). Significant knockdown of luciferase with siLuc was persistent from day 7 to day 9. The black arrows indicate the days of treatment. The mice were observed for 3 days before the treatment and 4 days after the treatment. \* = p<0.05 and \*\*\* = p<0.001**.** (F) Representative section of the corneas treated in with QN-Palm-POD-siRNA, stained with haematoxylin and eosin. No abnormality or signs of inflammation were observed in any treated cornea.

|  |  |  |
| --- | --- | --- |
| POD with siRNA | Dimension (nm) | Zeta-potential (mV) |
| Chol-POD in PBS | 150.8 ± 0.28 | +15.6 ± 0.8 |
| Palm-POD in PBS | 142.5 ±3.1 | +14.5 ± 1.8 |
| PLGA-PEG-POD in PBS | 127 ± 10.9 | +11.9 ± 3.5 |
| QN-Palm-POD in PBS | 107 ± 3.2 | +14.9 ± 4.2 |

**Table 1. POD dimensions and zeta-potentials.** POD:siRNA molar ratio was 140:1 for QN-Palm-POD and 35:1 for the other PODs

|  |  |  |
| --- | --- | --- |
| **Name** | **Structure** | **MW (g/mol)** |
| POD | CGGG[ARKKAAKA]4 | 3592.4 |
| Palm-POD | CH3-(CH2)14-CO-POD | 3829.9 |
| Chol-POD | C28H45O-CO-POD | 4004.1 |
| QN-Palm-POD | C66H100F6N12O6-CO-POD | 4873.0 |
| PLGA-PEG-POD | [C3H4O2]x[C2H2O2]y[C2H4O]zC9H11N2O3-POD | 29500-43500 |

**Table 2. POD structures and molecular weights**